



1 Dipolar Order Mediated $^1\text{H}\rightarrow^{13}\text{C}$ Cross-Polarization for Dissolution- 2 Dynamic Nuclear Polarization 3

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14 **Abstract.** Magnetic resonance imaging and spectroscopy often suffer from a low intrinsic sensitivity, which can in some cases be
15 circumvented by the use of hyperpolarization techniques. Dissolution-dynamic nuclear polarization offers a way of hyperpolarizing
16 ^{13}C spins in small molecules, enhancing their sensitivity by up to four orders of magnitude. This is usually performed by direct ^{13}C
17 polarization, which is straightforward but often takes more than an hour. Alternatively, indirect ^1H polarization followed by $^1\text{H}\rightarrow^{13}\text{C}$
18 polarization transfer can be implemented, which is more efficient and faster but is technically very challenging and hardly
19 implemented in practice. Here we propose to remove the main roadblocks of the $^1\text{H}\rightarrow^{13}\text{C}$ polarization transfer process by using
20 alternative schemes with: (i) less *rf*-power; (ii) less overall *rf*-energy; (iii) simple *rf*-pulse shapes; and (iv) no synchronized ^1H and
21 ^{13}C *rf*-irradiation. An experimental demonstration of such a simple $^1\text{H}\rightarrow^{13}\text{C}$ polarization transfer technique is presented for the case
22 of $[1-^{13}\text{C}]$ sodium acetate, and is compared with the most sophisticated cross-polarization schemes. A polarization transfer
23 efficiency of ~ 0.43 with respect to cross-polarization was realized, which resulted in a ^{13}C polarization of $\sim 8.7\%$ after ~ 10 minutes
24 of microwave irradiation and a single polarization transfer step.
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26 27 1 Introduction 28

29 Traditional magnetic resonance imaging (MRI) and spectroscopy (MRS) experiments usually suffer from low sensitivity.
30 Hyperpolarization techniques including dissolution-dynamic nuclear polarization (*d*DNP) can be used to highly polarize a large
31 variety of chemical systems and therefore enhance nuclear magnetic resonance (NMR) signals by several orders of magnitude
32 (Ardenkjær-Larsen et al., 2003). Various applications of *d*DNP have been demonstrated including the study of enzyme kinetics,
33 cell extracts and heteronuclear metabolomics (Bornet et al., 2014; Dumez et al., 2015; Bornet et al., 2016). Most *d*DNP applications
34 involve the use of weakly magnetic isotopes such as ^{13}C , but excessively long DNP timescales $\tau_{\text{DNP}}(^{13}\text{C})$ hinder efficient
35 polarization build-up and lead to extended experimental times. Intrinsically sensitive proton nuclear spins do not suffer from such
36 issues and can be polarized quickly and to a greater extent at low temperatures.

37 The use and optimization of cross-polarization (CP) under *d*DNP conditions (typ. at temperatures of about 1.2-1.6 K in
38 superfluid helium) provides a way to substantially boost ^{13}C polarizations and enhance build-up rates $1/\tau_{\text{DNP}}(^{13}\text{C})$ (by a factor of up
39 to 40) (Hartmann and Hahn, 1962; Pines et al., 1972; Jannin et al., 2011; Bornet et al., 2012; Batel et al., 2012; Bornet et al., 2013;
40 Vuichoud et al., 2016; Cavallès et al., 2018; Perez Linde, 2009). The technique requires intense B_1 -matching (typ. > 15 kHz) of
41 simultaneous ^1H and ^{13}C spin-locking radiofrequency (*rf*) fields throughout an optimized contact period (typ. > 1 ms). This CP-
42 DNP approach recently turned out to be key for the preparation of transportable hyperpolarization (Ji et al., 2017) where samples
43 are polarized in a CP equipped polarizer and then transported over extended periods (typ. hours or days) to the point of use.

44 This CP approach has been demonstrated on typical *d*DNP samples back in 2012 (Bornet et al., 2012), however, the technique
45 remains challenging today because of its methodological and technical complexity. Indeed, CP under *d*DNP conditions employs
46 sophisticated pulse sequences and involves high power and energy *rf*-pulses. Another drawback of CP-DNP is that it can hardly be



47 scaled-up to volumes larger than 500 μL , otherwise engendering detrimental arcing in the superfluid helium bath (Vinther et al.,
48 2019). Such scaling-up would be required for enabling parallel hyperpolarization of multiple transportable samples (Lipsø et al.,
49 2017), and for volumes >1 mL currently used for hyperpolarized human imaging (Nelson et al., 2013).

50 For hyperpolarizing larger sample volumes, alternative *rf*-sequences with reduced power requirements are desired. Lower
51 power alternatives to CP have previously been described in the literature (Vinther et al., 2019; Jeener and Broekaert, 1967; Vieth
52 and Yannoni, 1993; Emid et al., 1980; Zhang et al., 1993; Khitritin et al., 2011; Jeener et al., 1965; Redfield, 1969; Demco et al.,
53 1975; Kunitomo et al., 1974; Lee and Khitritin, 2008), which rely on indirect polarization transfer via proton dipolar order rather
54 than through a direct ^1H - ^{13}C Hartman-Hahn matching condition (Hartmann and Hahn, 1962).

55 The population of a Zeeman eigenstate for a spin-1/2 nucleus at thermal equilibrium ρ_{eq}^i is given as follows:
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$$57 \rho_{eq}^i = \frac{\exp\left\{-\frac{\hbar\omega_i}{k_B T}\right\}}{Z}, \quad (1)$$

58
59 where ω_i is the energy of the state for the spin of interest, T is the temperature and Z is a canonical partition function. In the high-
60 temperature limit, the spin density operator $\hat{\rho}_{eq}$ (which describes the state of an entire ensemble of spin-1/2 nuclei at thermal
61 equilibrium) is expressed by using a truncated Taylor series:
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$$63 \hat{\rho}_{eq} \simeq \hat{1} + \mathbb{B} \sum_i \hat{I}_{iz}, \quad (2)$$

64
65 where $\mathbb{B} = \hbar\omega_0/k_B T$, ω_0 is the nuclear Larmor frequency for the spins of interest and \hat{I}_{iz} is z -angular momentum operator for
66 spin i . The second term in Equation 2 corresponds to longitudinal magnetization. However, outside of the high-temperature
67 approximation higher order terms in the spin density operator expansion cannot be ignored:
68

$$69 \hat{\rho}_{eq} \simeq \hat{1} + \mathbb{B} \sum_i \hat{I}_{iz} + \frac{\mathbb{B}^2}{2} \sum_i \sum_j \hat{I}_{iz} \cdot \hat{I}_{jz}. \quad (3)$$

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71 The third term in Equation 3 reveals the presence of nuclear dipolar order (Fukushima and Roeder, 1981) which can be in principle
72 prepared by generating strongly polarized spin systems, such as those established through conducting *d*DNP experiments (Sugishita
73 et al., 2019). Such dipolar order can also be efficiently generated by suitable *rf*-pulse sequences, and ultimately used to transfer
74 polarization (Vinther et al., 2019; Jeener and Broekaert, 1967; Vieth and Yannoni, 1993; Emid et al., 1980; Zhang et al., 1993;
75 Khitritin et al., 2011; Jeener et al., 1965; Redfield, 1969; Demco et al., 1975; Kunitomo et al., 1974; Lee and Khitritin, 2008). For the
76 sake of simplicity, we will refer here to such polarization transfer schemes as *d*CP for dipolar order mediated cross-polarization.

77 In this Article, we revisit the concept of $^1\text{H} \rightarrow ^{13}\text{C}$ *d*CP polarization transfer and assess its efficiency in the context of *d*DNP
78 experiments at 1.2 K and 7.05 T. We show that for a sample of [$1\text{-}^{13}\text{C}$]sodium acetate, a ^{13}C polarization of $\sim 8.7\%$ can be achieved
79 after ~ 10 minutes of ^1H DNP and the use of a sole polarization transfer step. The overall *d*CP transfer efficiency is ~ 0.43 with
80 respect to the most sophisticated and efficient high power CP sequences available today. The experimental data presented indicate
81 that ^1H Zeeman order (\hat{I}_z) is first converted to ^1H - ^1H dipolar order ($\hat{I}_{iz} \cdot \hat{I}_{2z}$) and presumably subsequently converted to the desired
82 ^{13}C Zeeman order (\hat{S}_z). We show how the use of microwave gating (Bornet et al., 2016) is key to *d*CP as it improves the overall
83 efficiency by a factor more than ~ 2.3 .
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85 2 Methods

86 87 2.1 Sample Preparation and Freezing



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89 A solution of 3 M [^{13}C]sodium acetate in the glass-forming mixture $\text{H}_2\text{O}:\text{D}_2\text{O}:\text{glycerol-}d_8$ (10%:30%:60% v/v/w) was doped with
90 50 mM TEMPOL radical (all compounds purchased from *Sigma Aldrich*) and sonicated for ~ 10 minutes. This sample is referred
91 to as **I** from here onwards. A 100 μL volume of **I** was pipetted into a Kel-F sample cup and inserted into a 7.05 T prototype *Bruker*
92 *Biospin* polarizer equipped with a specialized *dDNP* probe and running *TopSpin 3.7* software. The sample temperature was reduced
93 to 1.2 K by submerging the sample in liquid helium and reducing the pressure of the variable temperature insert (VTI) towards
94 ~ 0.7 mbar.

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96 2.2 Dynamic Nuclear Polarization

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98 The sample was polarized by applying microwave irradiation at 197.648 GHz (positive lobe of the EPR line) with triangular
99 frequency modulation of amplitude $\Delta f_{\text{mw}} = 120$ MHz (Bornet et al., 2014) and rate $f_{\text{mod}} = 0.5$ kHz at a power of c.a. 100 mW.
100 Microwave gating was employed shortly before and during *dDNP* transfer experiments to allow the electron spin ensemble to
101 return to a highly polarized state, which happens on the timescale of the longitudinal electron relaxation time (typ. $T_{1e} = 100$ ms
102 with $P_e = 99.93\%$ under *dDNP* conditions) (Bornet et al., 2016). Consequently, the ^1H and ^{13}C relaxation times in the presence of
103 a *rf*-field are extended by orders of magnitude, allowing spin-locking *rf*-pulses to be much longer which significantly increases the
104 efficiency of nuclear polarization transfer.

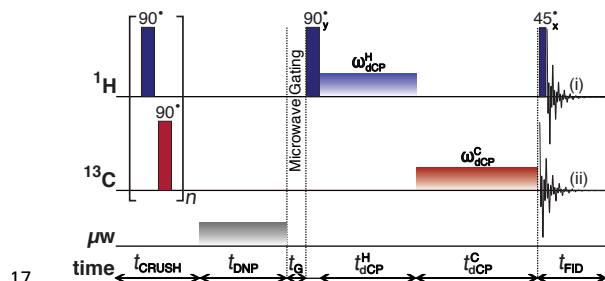
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106 2.3 Pulse Sequences

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108 In 1967 Jeener and Broekaert established the original *rf*-pulse sequence for creating and observing dipolar order in the solid-state
109 (Jeener and Broekaert, 1967). Since then, other *rf*-pulse sequences have been proposed in the literature, usually with improved
110 efficiency (Vinther et al., 2019; Vieth and Yannoni, 1993; Emid et al., 1980; Zhang et al., 1993; Khitrin et al., 2011; Jeener et al.,
111 1965; Redfield, 1969; Demco et al., 1975; Kunitomo et al., 1974; Lee and Khitrin, 2008). Herein, we are most interested in the *rf*-
112 pulse sequence introduced by Vieth and Yannoni (Vieth and Yannoni, 1993) which is particularly simple, easily generates proton
113 dipolar order and allows subsequent conversion to ^{13}C polarization. Figure 1 shows this sequence adapted for our *dDNP*
114 experiments. An electron-nuclear variant of this *rf*-pulse sequence has also been developed (Macho et al., 1991; Buntkowsky et al.,
115 1991).

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119 Figure 1: Schematic representation of the *dCP* *rf*-pulse sequence used for preparing and monitoring ^1H - ^1H dipolar order in **I**, and the conversion to ^{13}C
120 transverse magnetization. The experiments used the following parameters, chosen to maximize magnetization-dipolar order interconversion: $n = 250$; t_{DNP}
121 $= 5$ s; $t_G = 0.5$ s; $\omega_{\text{dcp}}^{\text{H}}/2\pi = 16.4$ kHz; $t_{\text{dcp}}^{\text{H}} = 25$ μs ; $\omega_{\text{dcp}}^{\text{C}}/2\pi = 13.2$ kHz; $t_{\text{dcp}}^{\text{C}} = 39$ ms. The ^1H and ^{13}C spin-locking *rf*-pulses have phase x . The $\pi/2$ crusher
122 *rf*-pulses use a thirteen-step phase cycle to remove residual magnetization at the beginning of each experiment: $\{0, \pi/18, 5\pi/18, \pi/2, 4\pi/9, 5\pi/18, 8\pi/9,$
123 $\pi, 10\pi/9, 13\pi/9, \pi/18, 5\pi/3, 35\pi/18\}$. The resonance offset was placed at the centre of the ^1H and ^{13}C NMR peaks.

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25 The *dCP rf*-pulse sequence operates as follows:

26 (i) A crusher sequence of 90° *rf*-pulses with alternating phases separated by a short delay (typ. 11 ms) repeated n times (typ. n
27 = 250) kills residual magnetization on both *rf*-channels;

28 (ii) The microwave source becomes active for a time t_{DNP} during which ^1H DNP builds-up;

29 (iii) The microwave source is deactivated and a delay of duration $t_G = 0.5$ s occurs before the next step, thus permitting the
30 electron spins to relax to their highly polarized thermal equilibrium state (Bornet et al., 2016);

31 (iv) A ^1H 90° *rf*-pulse followed by a $\pi/2$ phase-shifted spin-locking ^1H *rf*-pulse of amplitude $\omega_{\text{dCP}}^{\text{H}}$ and length $t_{\text{dCP}}^{\text{H}}$ converts ^1H
32 Zeeman polarization into ^1H - ^1H dipolar order;

33 (v) A ^{13}C square *rf*-pulse of amplitude $\omega_{\text{dCP}}^{\text{C}}$ and length $t_{\text{dCP}}^{\text{C}}$ presumably converts the ^1H - ^1H dipolar order into ^{13}C transverse
34 magnetization.

35 The NMR signal can be detected by using either: (i) a ^1H 45° *rf*-pulse followed by ^1H FID acquisition to monitor the remaining
36 proton dipolar order; or (ii) ^{13}C FID detection to observe the converted magnetization, see Figure 1.

37 The *dCP rf*-pulse sequence can be used in several variants:

38 *Variant #1*: Efficiency of ^1H - ^1H dipolar order preparation.

39 (a) ^1H observation by fixing $t_{\text{dCP}}^{\text{C}} = 0$ ms and varying $\omega_{\text{dCP}}^{\text{H}}$ and $t_{\text{dCP}}^{\text{H}}$ (Figure 2a);

40 (b): ^{13}C observation by fixing $t_{\text{dCP}}^{\text{C}}$ and $\omega_{\text{dCP}}^{\text{C}}$ (typ. to an optimal value) and varying $\omega_{\text{dCP}}^{\text{H}}$ and $t_{\text{dCP}}^{\text{H}}$ (Figure 2c).

41 *Variant #2*: Efficiency of ^1H - ^1H dipolar order conversion to ^{13}C magnetization.

42 (a): ^{13}C observation by fixing $\omega_{\text{dCP}}^{\text{H}}$ and $t_{\text{dCP}}^{\text{H}}$ (typ. to an optimal value) and varying $\omega_{\text{dCP}}^{\text{C}}$ and $t_{\text{dCP}}^{\text{C}}$ (Figure 3a);

43 (b): ^1H observation by fixing $\omega_{\text{dCP}}^{\text{H}}$ and $t_{\text{dCP}}^{\text{H}}$ (typ. to an optimal value) and varying $\omega_{\text{dCP}}^{\text{C}}$ and $t_{\text{dCP}}^{\text{C}}$ (Figure 4a).

44 The amplitudes of the ^1H and ^{13}C *dCP rf*-pulses ($\omega_{\text{dCP}}^{\text{H}}$ and $\omega_{\text{dCP}}^{\text{C}}$, respectively) were optimized iteratively until the intensity of
45 the resulting NMR signals could not be improved further, see the Electronic Supplementary Material (ESM) for more details.

46 In the case of proton *rf*-channel acquisition, data points were acquired with a two-step phase cycle, in which the phase of the
47 90_y *rf*-pulse and the digitizer were simultaneously changed by 180° in successive transients, to remove spurious signals generated
48 by longitudinal magnetization accrued during the *dCP rf*-pulses. A dispersive lineshape was observed as a result of the phase cycle,
49 which is characteristic of dipolar spin order. The resulting ^1H NMR spectrum was phase corrected to yield an absorptive lineshape.

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51 **3 Results**

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53 **3.1 ^1H - ^1H Dipolar Order Preparation**

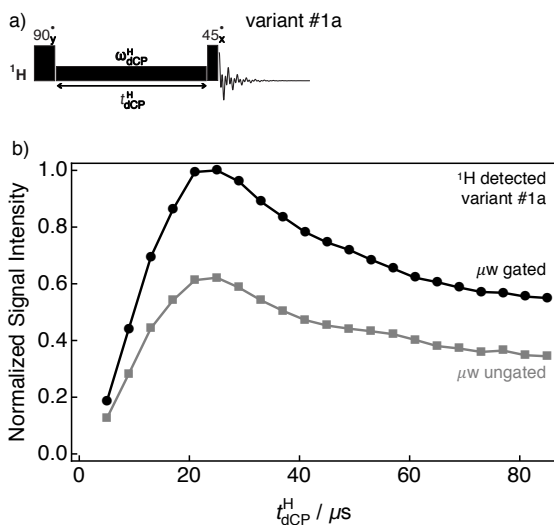
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55 ^1H monitored optimization for the generation of ^1H - ^1H dipolar order as a function of the *dCP* ^1H *rf*-pulse duration $t_{\text{dCP}}^{\text{H}}$ was
56 performed by using *variant #1a* of the *dCP* sequence shown in Figure 2a. Experimental results demonstrating the preparation of
57 ^1H - ^1H dipolar order under *variant #1a* of the *dCP* sequence are shown in Figure 2b. The integrals plotted were acquired directly
58 on the ^1H *rf*-channel using $\omega_{\text{dCP}}^{\text{H}}/2\pi = 16.4$ kHz either with or without microwave gating (black circles and grey squares,
59 respectively). In both cases, the NMR signal grows until a maximum signal intensity, which corresponds to the optimal preparation
60 of proton dipolar order, is reached at $t_{\text{dCP}}^{\text{H}} \approx 25$ μs , after which the signal decays towards a stable plateau on a longer timescale.
61 However, in the case that microwave gating is removed, the signal intensity is reduced. This is due to depolarization (microwave
62 saturation) of the electron spins, resulting in a detrimental enhancement of the paramagnetic relaxation contribution to nuclear spin
63 relaxation. These results suggest that microwave gating improves the conversion of ^1H magnetization to ^1H - ^1H dipolar order by a
64 factor of at least ~ 1.6 .

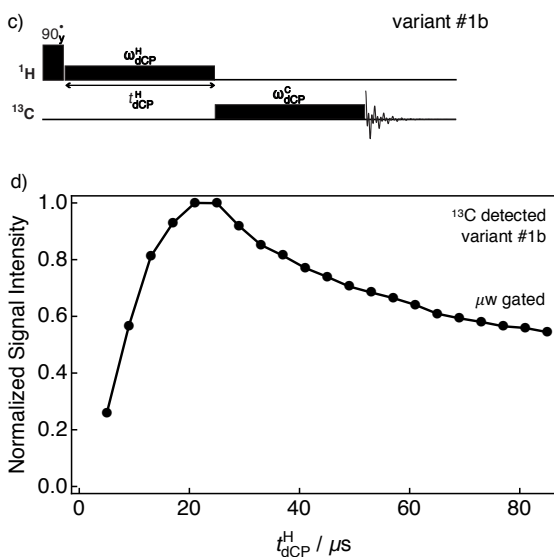
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Figure 2: Simplified schematic representations of (a) *variant #1a* and (c) *variant #1b* of the *dCP rf-pulse* sequence. Experimental (b) ^1H and (d) ^{13}C NMR signal intensities of I as a function of the ^1H *dCP rf-pulse* duration $t_{\text{dCP}}^{\text{H}}$ acquired at 7.05 T (^1H nuclear Larmor frequency = 300.13 MHz, ^{13}C nuclear Larmor frequency = 75.47 MHz) and 1.2 K with two transients per data point. The traces have the same overall form, and plateau over a period of 200 μs (data not shown).

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^{13}C monitored optimization for the build-up of ^1H - ^1H dipolar order was performed by using *variant #1b* of the *dCP rf-pulse* sequence demonstrated in Figure 2c. In Figure 2d the experimental integrals are plotted against the *dCP* ^1H *rf-pulse* duration $t_{\text{dCP}}^{\text{H}}$ and were acquired on the ^{13}C *rf-channel* with $\omega_{\text{dCP}}^{\text{H}}/2\pi = 16.4$ kHz, $\omega_{\text{dCP}}^{\text{C}}/2\pi = 13.2$ kHz and $t_{\text{dCP}}^{\text{C}} = 39$ ms (black circles). It is important to note that the maximum is identical whether the NMR signal is observed on the ^1H *rf-channel* by using *variant #1a* or on the ^{13}C *rf-channel* by using *variant #1b*, and more generally that the two traces have the same shape and optimum. This shows that ^{13}C transverse magnetization from *dCP* is proportional to the ^1H - ^1H dipolar order initially prepared.

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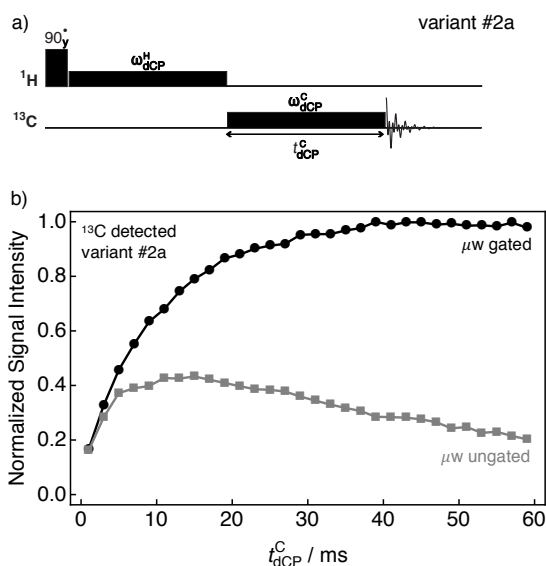


3.2 ^1H - ^{13}C Polarization Transfer

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38 Figure 3b shows how ^{13}C magnetization is built-up by employing *variant #2a* the *dCP rf-pulse* sequence, see Figure 3a. The
 39 experimental integrals of the ^{13}C signal are plotted against the ^{13}C *dCP rf-pulse* duration $t_{\text{dCP}}^{\text{C}}$ with (black circles) and without (grey
 40 squares) microwave gating.

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46 **Figure 3:** (a) Simplified schematic representation of *variant #2a* of the *dCP rf-pulse* sequence. (b) Experimental ^{13}C NMR signal intensity of I as a function
 47 of the *dCP rf-pulse* duration $t_{\text{dCP}}^{\text{C}}$ acquired at 7.05 T (^1H nuclear Larmor frequency = 300.13 MHz, ^{13}C nuclear Larmor frequency = 75.47 MHz) and 1.2
 48 K with two transients per data point.

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50 The black trace corresponds to the growth of the ^{13}C NMR signal. A maximum is reached at $t_{\text{dCP}}^{\text{C}} \approx 39$ ms, with $\omega_{\text{dCP}}^{\text{C}} = 13.2$
 51 kHz. The polarization transfer efficiency is relatively robust with respect to the amplitude of the ^{13}C *dCP rf-pulse* $\omega_{\text{dCP}}^{\text{C}}$, see the
 52 ESM for more details. A wildly different behaviour is observed in the case where the microwave source is not gated. In this
 53 instance, a maximum signal intensity occurs at $t_{\text{dCP}}^{\text{C}} \approx 15$ ms, with the detectable ^{13}C signal decreasing past this point. The ratio
 54 between the maximum data points is ~ 2.3 , and indicates a large ^{13}C enhancement afforded by microwave gating.

55 It is worth noting that the duration of the ^{13}C *dCP rf-pulse* is considerably longer, more than three orders of magnitude, than the
 56 ^1H *dCP rf-pulse* lengths. Reasons for this are examined in the discussion section below.

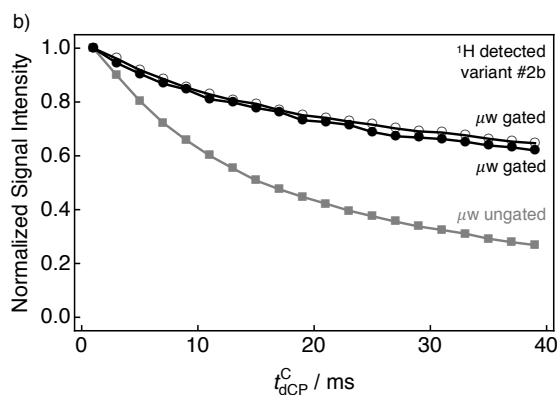
57 Figure 4b details how in *variant #2b* of the *dCP rf-pulse* sequence (Figure 4a) the ^1H NMR signal vanishes as the ^{13}C *dCP rf-*
 58 pulse generates ^{13}C transverse magnetization. The experimental integrals of the ^1H detected NMR signals are plotted against the
 59 ^{13}C *dCP rf-pulse* duration $t_{\text{dCP}}^{\text{C}}$ with $\omega_{\text{dCP}}^{\text{C}} = 0$ kHz (black open circles) and $\omega_{\text{dCP}}^{\text{C}} = 13.2$ kHz (black circles) both with microwave
 60 gating, and with $\omega_{\text{dCP}}^{\text{C}} = 13.2$ kHz (grey squares) without microwave gating.

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16 **Figure 4:** (a) Simplified schematic representation of *variant #2b* of the *dCP* *rf*-pulse sequence. (b) Experimental ^1H NMR signal intensity of I as a function
17 of the ^{13}C *dCP* *rf*-pulse duration t_{dCP}^C acquired at 7.05 T (^1H nuclear Larmor frequency = 300.13 MHz, ^{13}C nuclear Larmor frequency = 75.47 MHz) and
18 1.2 K with two transients per data point. The experimental traces were recorded by using the following amplitudes for the ^{13}C *dCP* *rf*-pulse ω_{dCP}^C : Black
19 open circles: $\omega_{dCP}^C = 0$ kHz; Black filled circles: $\omega_{dCP}^C = 13.2$ kHz; Grey squares: $\omega_{dCP}^C = 13.2$ kHz. All signal amplitudes were normalized to the first data
20 point.

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22 The curves show how ^1H - ^1H dipolar order decays towards thermal equilibrium mainly through relaxation and is not significantly
23 affected by the presence of the ^{13}C *dCP* *rf*-pulse generating ^{13}C magnetization. The difference between the two black traces might
24 however indicate the quantity of ^1H - ^1H dipolar order converted into ^{13}C magnetization. The small difference is just a few percent,
25 indicating that only a very small portion of the ^1H - ^1H dipolar order might be used (and be useful) to produce hyperpolarized ^{13}C
26 magnetization. This could be explained by the large excess of ^1H spins compared with ^{13}C spins in our sample (a factor of ~ 6.2).
27 A lack of microwave gating (grey squares) significantly compromises the generation of ^{13}C polarization, as seen in Figure 3b.

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29 3.3 Comparison to Cross-Polarization

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31 The performance efficiency of the *dCP* *rf*-pulse sequence was compared to a traditional CP experiment (Hartmann and Hahn, 1962;
32 Pines et al., 1972; Jannin et al., 2011; Bornet et al., 2012; Batel et al., 2012; Bornet et al., 2013; Vuichoud et al., 2016; Cavaillès
33 et al., 2018; Perez Linde, 2009), which is described in the ESM along with a *rf*-pulse sequence diagram and all optimized
34 parameters. Experiments employed 640 s of direct ^1H DNP at 1.2 K prior to polarization transfer to the ^{13}C heteronucleus.

35 The power requirements for polarization transfer are dependent upon the *rf*-pulse sequence used and the capabilities of the
36 *dDNP* probe. In general, the peak power for the ^{13}C *dCP* *rf*-pulse is ~ 5.4 times lower than required for CP. However, the ^{13}C *dCP*
37 *rf*-pulse is active for a duration ~ 5.6 times longer than that of CP, and hence the overall deposited *rf*-pulse energy is approximately
38 the same for both *rf*-pulse sequences. Notwithstanding, the moderately lower ^{13}C *dCP* *rf*-pulse power is highly advantageous, e.g.
39 decreased likelihood of probe arcing events within the superfluid helium bath. The benefit of employing the *dCP* *rf*-pulse sequence
40 becomes even more apparent when examining the proton *rf*-pulse durations needed for ^1H - ^{13}C polarization transfer. Although the
41 peak powers of both *rf*-pulse sequences are similar, the duration of the ^1H *dCP* *rf*-pulse is a factor of 280 times shorter than that
42 recommended for adequate CP. This is advantageous in the case that the B_1 -field produced by the *dDNP* probe is weak (e.g. due to
43 large sample constraints) or is unstable at higher ^1H *rf*-pulse powers for sufficiently long durations.

44 The CP *rf*-pulse sequence achieved a ^{13}C polarization level of $P(^{13}\text{C}) \approx 20.4\%$ after a single CP contact. ^{13}C polarization levels
45 in excess of 60% are anticipated by using a multiple CP contact approach (Jannin et al., 2011; Bornet et al., 2012; Batel et al., 2012;
46 Bornet et al., 2013; Vuichoud et al., 2016; Cavaillès et al., 2018; Perez Linde, 2009). In comparison, the integral of the *dCP*-filtered
47 NMR signal maximum is scaled by a factor of ~ 0.43 , indicating a ^{13}C polarization of $P(^{13}\text{C}) \approx 8.7\%$. This is consistent with



48 previous results reported in the literature (Perez Linde, 2009; Vinther et al., 2019). Strategies to further improve the *dCP* efficiency
49 are presented in the discussion section.

50

51 **4 Discussion**

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53 The results presented in Figure 2b and Figure 2d show how the achieved ^{13}C polarization is directly proportional to the quantity of
54 ^1H - ^1H dipolar order initially prepared by the ^1H *dCP* *rf*-pulse. However, even if the ^{13}C polarization closely follows the shape of
55 the proton dipolar order creation profile, this does not constitute irrefutable proof that the ^{13}C polarization originates from the
56 proton dipolar order reservoir itself. Other, more-complex forms of nuclear spin order might be involved. Moreover, it is feasible
57 that an intermediate reservoir exists, such as non-Zeeman spin order of the ^{13}C heteronucleus.

58 As seen in Figure 3b, it is interesting to note that the duration of the ^{13}C *dCP* *rf*-pulse is considerably longer, more than three
59 orders of magnitude, than the ^1H *dCP* *rf*-pulse duration. The reason is the relative sizes of the dipolar couplings which control the
60 preparation and transfer processes of ^1H - ^1H dipolar order. The generation of dipolar order involves only proton spins, which possess
61 a magnetogyric ratio ~ 4 times greater than for ^{13}C spins and consequently larger dipolar couplings, which scale as the product of
62 the magnetogyric ratios for the two spins involved. This results in a short time to convert ^1H magnetization to ^1H - ^1H dipolar order.
63 Conversely, the transfer of ^1H - ^1H dipolar order to ^{13}C nuclei would certainly demand ^1H - ^{13}C dipolar couplings.

64 The duration of the ^{13}C *dCP* *rf*-pulse is a factor of ~ 5.6 longer than required for optimized conventional CP (see the ESM for
65 more details). The extended duration of the ^{13}C *dCP* *rf*-pulse could be conceivably explained by assuming that the ^1H spins closest
66 to the ^{13}C spin do not participate in the polarization transfer process since the ^1H - ^1H dipolar order preparation is perturbed by the
67 presence of the ^{13}C spin during the ^1H *dCP* *rf*-pulse. It is also possible that two dipolar coupled protons are separated by a difference
68 in chemical shift which matches the frequency of a ^{13}C spin the rotating frame allowing an exchange of energy. Such events are
69 similar to the cross-effect in DNP (Kessenikh et al., 1963) but are likely to be of lower probability, leading to an increased ^{13}C *dCP*
70 *rf*-pulse duration.

71 Not only is the polarization transfer process long, but it is also weaker than what is usually realized with optimized CP, since
72 we obtain $P(^{13}\text{C}) \approx 8.7\%$ rather than $P(^{13}\text{C}) \approx 20.4\%$ in a single CP step on the same sample. Although the amplitude $\omega_{\text{dCP}}^{\text{H}}$ and
73 duration $t_{\text{dCP}}^{\text{H}}$ of the proton dipolar order creation *rf*-pulse were carefully optimized before experimental implementation, we
74 nevertheless believe there is still room for improvement in preparing high quantities of proton dipolar order. The performance of
75 the *dCP* *rf*-pulse sequence could be enhanced by adopting the following strategies: (i) employing shaped *rf*-pulses; (ii)
76 implementing a multiple *dCP* transfer approach; (iii) optimizing the protonation level of the DNP glassing solution; (iv) exploiting
77 deuterated molecular derivatives; (v) avoiding large quantities of methyl groups which may act as dipolar order relaxation sinks
78 due to their inherent rotation (which remains present at liquid helium temperature); and (vi) changing the molecule [$1\text{-}^{13}\text{C}$]sodium
79 acetate for another spin system with different ^1H - ^{13}C coupling strengths (e.g. simply using [$2\text{-}^{13}\text{C}$]sodium acetate).

80 Today's performances on our current 'standard' DNP sample are rather poor compared to CP, however, there are reasons to
81 think that further improvements through advanced *rf*-pulse schemes and revised sample formulations will be possible in the future,
82 and that *dCP* may become a viable alternative to CP. This will be particularly relevant to the cases of: (i) issues related to probe
83 arcing in the superfluid helium bath which precludes the use of conventional CP experiments; (ii) increased sample volumes, e.g.
84 in human applications; and (iii) hyperpolarization of insensitive nuclear spins, e.g. ^{89}Y nuclei cannot be polarized easily via
85 traditional CP experiments due to unfeasible CP matching conditions on the heteronuclear *rf*-channel. Other alternatives to the CP
86 approach also exist but are theoretically less efficient, such as low magnetic field nuclear thermal mixing (Gadian et al., 2012)
87 which relies on energy conserving mutual spin-flips in overlapping NMR lineshapes to polarize heteronuclei in solid samples (Peat
88 et al., 2016).

89



90 **5 Conclusions**

91

92 $^1\text{H}\rightarrow^{13}\text{C}$ polarization transfer occurs by employing *rf*-pulse methods which operate under *d*DNP conditions. This supposedly
93 involves an intermediate reservoir of dipolar order, which governs the polarization transfer process. The spin dynamics of dipolar
94 order mediated cross-polarization (*d*CP) were found to significantly depend on the presence of microwave gating. A maximum ^{13}C
95 polarization of ~8.7% was observed after ~10 minutes of microwave irradiation and a lone polarization step, which corresponds to
96 a *d*CP polarization transfer efficiency of ~0.43 with respect to optimized conventional CP. These results are promising for future
97 applications of polarization conversion methods in the context of low power $^1\text{H}\rightarrow\text{X}$ polarization transfer to insensitive nuclei (in
98 particular for very low magnetogyric ratios), with minimized probe arcing and potentially large sample volumes, paving the way
99 to the use of $^1\text{H}\rightarrow\text{X}$ polarization transfer in clinical (human-dose) contexts.

100

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102

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115

116 **Author Contributions**

117

118 SJE performed experiments and co-wrote the manuscript, SFC/QC/OC/AB performed experiments, MC built parts of the
119 experimental apparatus, and SJ conceived the idea and co-wrote the manuscript.

120

121 **Competing Interests**

122

123 The authors declare no competing interests.

124

125 **References**

126

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