Solid-State ¹H Spin Polarimetry by ¹³CH₃ Nuclear Magnetic Resonance

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Abstract. Dissolution-dynamic nuclear polarization is used to prepare proton polarizations approaching unity. At present, ¹H 11 12 polarization quantification remains fastidious due to the requirement of measuring thermal equilibrium signals. Lineshape 13 polarimetry of solid-state nuclear magnetic resonance spectra is used to determine several useful properties regarding the spin system under investigation. In the case of highly polarized nuclear spins, such as those prepared under the conditions of dissolution-14 dynamic nuclear polarization experiments, the absolute polarization of a particular isotopic species within the sample may be 15 16 directly inferred from the characteristics of the corresponding resonance lineshape. In situations where direct measurements of polarization are complicated by deleterious phenomena, indirect estimates of polarization using coupled heteronuclear spins prove 17 informative. We present a simple analysis of the ¹³C spectral lineshape of [2-¹³C]sodium acetate based on the normalized deviation 18 of the centre of gravity of the ¹³C peaks, which can be used to indirectly evaluate the proton polarization of the methyl group moiety 19 20 and very likely the entire sample in the case of rapid and homogeneous ¹H-¹H spin diffusion. For the case of positive microwave 21 irradiation, ¹H polarization was found to increase with an increasing normalized centre of gravity deviation. These results suggest 22 that, as a dopant, $[2-^{13}C]$ sodium acetate could be used to indirectly gauge ¹H polarizations in standard sample formulations, which 23 is potentially advantageous for: (i) samples polarized in commercial dissolution-dynamic nuclear polarization devices that lack ¹H 24 radiofrequency hardware; (ii) measurements that are deleteriously influenced by radiation damping or complicated by the presence 25 of large background signals; and (*iii*) situations where the acquisition of a thermal equilibrium spectrum is not feasible.

28 1 Introduction

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Classical nuclear magnetic resonance (NMR) experiments produce inherently weak signals. The severely limiting low intrinsic sensitivity of the technique can be enhanced by up to four orders of magnitude by employing a wide range of routinely used hyperpolarization methodologies (Ardenkjær-Larsen et al., 2003; Hirsch et al., 2015; Dale and Wedge, 2016; Meier 2018; Kouřil et al, 2019). The significantly boosted NMR signal intensities from metabolites hyperpolarized by implementing a dissolutiondynamic nuclear polarization (*d*DNP) approach have been used in the characterization of cancer in human patients (Nelson et al, 2013; Chen et al, 2020; Gallagher et al, 2020).

To hyperpolarize nuclear spins via the *d*DNP approach, the spin system of interest is co-frozen in a mixture of aqueous solvents and glassing agents with a carefully chosen paramagnetic radical species (Abragam and Goldman, 1978). The *d*DNP-compatible solution is subsequently frozen at liquid helium temperatures (where the solvent matrix forms a glass) inside a magnetic field and is irradiated with slightly non-resonant (with respect to the electron spin transition) microwaves, which transfer the high electron spin polarization to the nuclear spins of interest (Kundu et al, 2019).

Hyperpolarization of methyl group moieties by *d*DNP has led to some unusual effects including the generation of long-lived
spin order, which is revealed in the liquid-state upon dissolution of the material from cryogenic conditions (Meier et al, 2013; Roy
et al, 2015; Dumez et al, 2017; Elliott et al, 2018). Solid-state NMR of highly polarized nuclear spins has previously been utilized
to infer the sample polarization level and, in suitable cases, the quantity of long-lived spin order established (Elliott et al, 2018;
Waugh et al, 1987; Kuhns et al, 1989; Marohn et al, 1995; Kuzma et al, 2013; Mammoli et al, 2015; Willmering et al, 2017;

Aghelnejad et al, 2020). To the best of our knowledge, the solid-state NMR spectra of strongly polarized methyl groups have not
 shown any significant features which may be used for a clear lineshape analysis.

In this Communication, we propose that the ¹³C NMR lineshape of [2-¹³C]sodium acetate can be used to indirectly quantify the ¹H polarization of the methyl group spins. Furthermore, since ¹H-¹H spin diffusion rapidly achieves a homogeneous proton polarization across the entire sample, the ¹H polarization level of the whole sample is therefore likely to be reflected by the ¹H polarization of the methyl group moiety. We analyse the experimental ¹³C NMR spectra acquired for different ¹H polarizations and herein present a straightforward approach to indirectly quantify the ¹H polarization based on the ¹³C NMR peak normalized deviation of the centre of gravity (CoG). ¹H polarization was observed to increase with an increasing ¹³C NMR peak CoG deviation (case of positive microwave irradiation).

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2. Methods

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58 2.1. Sample Preparation

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A solution of 3 M [2^{-13} C]sodium acetate in the glass-forming mixture H₂O/D₂O/glycerol-*d*₈ (1/3/6 *v/v/v*) was doped with 50 mM TEMPOL radical (all compounds purchased from *Sigma Aldrich*) and sonicated for ~10 minutes. Paramagnetic TEMPOL radicals were chosen to polarize ¹H spins most efficiently under our *d*DNP conditions.

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64 2.2. Sample Freezing

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A 100 μ L volume of the above sample was pipetted into a Kel-F sample cup and inserted into a 7.05 T prototype *Bruker Biospin* polarizer equipped with a specialized *d*DNP probe, including a background-free radiofrequency (*rf*) coil insert (Elliott et al, 2021), running *TopSpin 3.5* software. The sample temperature was reduced to 1.2 K by submerging the sample in liquid helium and reducing the pressure of the variable temperature insert (VTI) towards ~0.7 mbar.

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71 2.3. Dynamic Nuclear Polarization

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The 100 μ L of sample was polarized by applying microwave irradiation at $f_{\mu w} = 197.616$ GHz (positive lobe of the DNP enhancement profile) or $f_{\mu w} = 198.192$ GHz (negative lobe of the DNP enhancement profile) with triangular frequency modulation (Bornet et al, 2014) of amplitude $\Delta f_{\mu w} = \pm 136$ MHz or $\Delta f_{\mu w} = \pm 112$ MHz, respectively, and rate $f_{mod} = 0.5$ kHz at a power of ca. 125 mW at the output of the microwave source (value given by the provider of our microwave source *VDI/AMC 705*) and ca. 30 mW reaching the DNP cavity (evaluated by monitoring the helium bath pressure, see Section 2.4), which were optimized prior to commencing experiments to achieve the highest possible level of ¹H polarization.

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80 2.4. Microwave Power Evaluation

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The microwave power reaching the DNP cavity was determined by comparison with the heating from a resistor in the liquid helium bath and calibrating how much the bath pressure increases vs. microwave power. In practice, the measurement was performed as follows:

85 (*i*) The VTI was filled with liquid helium and pumped down to 0.65 mbar, corresponding to 1.2 K;

(*ii*) The change of pressure when turning on a resistive heater or the microwave source for 120 s was monitored. The pressure
 plateaus after approximatively 60 s;

88 (*iii*) The pressure difference between the base pressure and that under the effect of the resistive heater or the microwave source 89 ΔP_{mbar} is calculated.

All measurements were performed ensuring that the liquid helium level in the VTI was not varying by more than a few centimetres: the microwave cavity was immersed under 5-10 cm of liquid helium. The measurements performed using the resistive heater with power P_{heater} are used to plot a calibration curve P_{heater} vs. ΔP_{mbar} with slope *a*. The deposited microwave power in the cavity is then obtained by computing $P_{\text{microwave}} = a\Delta P_{\text{mbar}}$.

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95 2.5. Polarization Build-Ups

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To monitor ¹³C NMR spectral lineshapes with satisfactory signal-to-noise ratios (SNRs), ¹³C polarization must first be built-up by using a succession of optimized cross-polarization (CP) contact *rf*-pulses. Then, to observe changes in the lineshape of ¹³C NMR spectra acquired as the ¹H polarization builds up from the thermal to DNP equilibrium, we employed a series of ¹H saturating *rf*pulses followed by microwave activation, a small flip-angle *rf*-pulse and ¹³C NMR signal detection, as shown by the *rf*-pulse sequence shown in Figure 1. The build-up of ¹³C polarization throughout the microwave irradiation period was tracked by engaging the following experimental procedure:

.03 (i) A saturating sequence of 90° *rf*-pulses with alternating phases separated by a short delay (typ. 11 ms) repeated *n* times (typ.

.04 n = 50 kills residual magnetization on both *rf*-channels;

.05 (*ii*) The microwave source becomes active and ¹H polarization builds up;

- .06 (*iii*) The ¹³C Zeeman magnetization trajectory is minimally perturbed by the application of a small flip-angle *rf*-pulse (typ. β =
- .07 3.5°) used for detection, which is then followed by a short acquisition period (typ. $t_{FID} = 1 \text{ ms}$);

.08 (iv) ¹H DNP builds up during a time t_{DNP}^1 (typ. $t_{\text{DNP}}^1 = 30$ s);

.09 (v) Stages *iii-iv* are cycled m times (typ. m = 6) in order to monitor the evolution of the ¹³C polarization (between CP steps);

.10 (vi) The microwave source is gated, and a delay of duration $t_G = 0.5$ s occurs, see Section 2.6, thus permitting the electron spins

.11 to relax to their highly polarized thermal equilibrium state before the next CP step (Bornet et al, 2016);

- .12 (*vii*) Two synchronized adiabatic half-passages (AHPs) simultaneously produce transverse magnetization for all pulsed spin
 .13 species;
- .14 (*viii*) The nuclear magnetization is subsequently spin-locked on both *rf*-channels (typically by a high power *rf*-pulse with a .15 nutation frequency on the order of 15 kHz and a duration between 1-10 ms) and ${}^{1}\text{H}\rightarrow{}^{13}\text{C}$ polarization transfer occurs (Bornet et al, .16 2016);
- .17 (*ix*) A second pair of harmonized AHPs (operating with reverse chronology) restores Zeeman magnetization on each *rf*-channel; .18 (*x*) Stages *ii-ix* are repeated in *L* units (typ. L = 8) to periodically transfer ¹H Zeeman polarization to ¹³C nuclear spins;
- .19 (xi) A second saturating sequence of 90° rf-pulses with alternating phases separated by a short delay (typ. 11 ms) repeated n
- .20 times (typ. n = 50) kills residual magnetization on the ¹H *rf*-channel only;
- .21 (*xii*) The microwave source reactivates;
- .22 (*xiii*) The ¹³C Zeeman magnetization trajectory is minimally perturbed by the application of a small flip-angle *rf*-pulse (typ. β
- .23 = 3.5°) used for detection, which is then followed by a short acquisition period (typ. $t_{FID} = 1 \text{ ms}$);
- .24 (xiv) ¹H DNP builds up during a time t_{DNP}^2 (typ. $t_{DNP}^2 = 5$ s);
- .25 (*xv*) Stages *xiii*-*xiv* are cycled *p* times (typ. p = 80) to monitor the evolution of the ¹³C NMR spectra as a function of the ¹H polarization build-up with sufficient SNR.
- .20 polarization bund up with sufficient brick.
 - .27 Further details regarding multiple-contact CP *rf*-pulse sequence operation are given elsewhere (Bornet et al, 2016). It should be
 - .28 stressed that the use of CP is purely optional, and in most cases its use will be dictated by the *rf*-hardware available. We use CP

here simply as a means to offer greater SNRs for ¹³C NMR signal detection. Given the level of sample deuteration, at 6.7 T and
 with microwave modulation suitable SNRs can also be achieved with direct ¹³C DNP (Chen et al., 2013).

.31 Since it is unlikely that the ¹³C NMR lineshape is significantly influenced by the ¹³C polarization, we can afford not to diminish .32 the ¹³C NMR signal intensity by a sequence of ¹³C saturating *rf*-pulses on the ¹³C *rf*-channel at stage *xi* to maintain high SNRs. The .33 small *rf*-pulse flip angles are necessary to preserve the ¹H and ¹³C polarizations throughout the course of the build-up experiment.

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Figure 1: Schematic representation of the *rf*-pulse sequence used to accrue ¹³C polarizations and monitor ¹³C lineshapes as a function of the ¹H polarization. The experiments used the following key parameters chosen to maximize the efficiency of the *rf*-pulse sequence: n = 50; $\beta = 3.5^{\circ}$; m = 6; $t_{DNP}^1 = 30$ s; L = 8; $t_G = 0.5$ s; p = 80; and $t_{DNP}^2 = 5$ s. AHP = adiabatic half-passage. AHP sweep width = 100 kHz. The $\pi/2$ saturating *rf*-pulses used an empirically optimized thirteen-step phase cycle to remove residual magnetization at the beginning of each experiment: $\{0, \pi/18, 5\pi/18, \pi/2, 4\pi/9, 5\pi/18, 8\pi/9, \pi, 10\pi/9, 13\pi/9, \pi/18, 5\pi/3, 35\pi/18\}$. The resonance offset was placed at the most intense peak of the ¹H and ¹³C NMR spectra.

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.43 2.6. Microwave Gating

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Microwave gating was employed shortly before and during CP experiments to allow the electron spin ensemble to return to a highly polarized state, which happens on the timescale of the longitudinal electron relaxation time (typ. $T_{1e} = 100$ ms with $P_e = 99.93\%$ under our experimental *d*DNP conditions) (Bornet et al, 2016). Microwave gating hence provides a way to strongly attenuate paramagnetic relaxation, and consequently the ¹H and ¹³C $T_{1\rho}$ relaxation time constants in the presence of an *rf*-field are extended by orders of magnitude. This allows spin-locking *rf*-pulses to be much longer, which significantly increases the efficiency of nuclear polarization transfer.

- .52 3. Results
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.54 **3.1.** ¹³C CP Build-Ups and Decays

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The CP build-up curves for the 13 C polarizations P_{C} as a function of the 14 H DNP time t_{DNP} for both positive and negative microwave .56 irradiation are shown in Figure 2. The ¹³C polarizations $P_{\rm C}$ were accrued by employing the *rf*-pulse sequence shown in Figure 1. .57 The ¹³C polarizations $P_{\rm C}$ ultimately reached $P_{\rm C} \simeq 40.6\%$ and $P_{\rm C} \simeq -46.8\%$ after 8 CP transfers and 24 minutes of positive and .58 negative microwave irradiation, respectively. The achieved levels of ${}^{13}C$ polarization P_C are lower than those previously reported .59 in the literature (Bornet et al, 2016), but were not further optimized since only the ¹³C NMR lineshape was of interest in this study .60 as a probe for absolute ¹H polarization. This is inconsequential for the current study since sufficient SNRs on the order of ~965 and .61 .62 ~1244 were achieved for the cases of positive and negative microwave irradiation, respectively. After this point, *i.e.*, beyond the vertical dashed line (¹H DNP time = 24 mins), a slow and partial decay of the ${}^{13}C$ NMR signal intensity towards a pseudo-.63 equilibrium is observed, see Figure 2. This ¹³C NMR signal decay is not a problem in general since the ¹³C NMR signal remains .64 sufficiently intense as to allow clear measurement of the ¹³C NMR lineshape with high accuracy. .65

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Figure 2: Experimental ¹³C polarization $P_{\rm C}$ CP build-up curves and subsequent ¹³C signal decays as a function of ¹H DNP time acquired at 7.05 T (¹H nuclear Larmor frequency = 300.13 MHz, ¹³C nuclear Larmor frequency = 75.47 MHz) and 1.2 K with a single transient per data point. The presented data were acquired by using the *rf*-pulse sequence depicted in Figure 1. Black filled squares: Positive microwave irradiation; Black empty squares: Negative microwave irradiation. The vertical dashed line denotes the ¹H DNP time at which the ¹H NMR signal was destroyed by a second series of saturating *rf*-pulses (as shown by the *rf*-pulse sequence illustrated in Figure 1).

.75 **3.2.** ¹³C NMR Spectra

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Figure 3 shows the relevant part of the experimental ¹³C NMR spectra acquired with a small flip angle *rf*-pulse ($\beta = 3.5^{\circ}$) at two different ¹H DNP times. The ¹³C NMR spectra in Figure 3 were acquired by using the *rf*-pulse sequence shown in Figure 1. The initial ¹³C NMR spectrum (acquired at 24 mins) is a single peak with a linewidth at full-width half-maximum height (FWHM) of ~10.9 kHz. The ¹³C NMR lineshape is relatively symmetrical and has no obvious defining features, see Figure 3a. Small peak contributions to the ¹³C NMR spectrum are observed towards the baseline, including one environment shifted as much as ca. -300ppm. This spectrum corresponds to a low level of ¹H polarization ($|P_H| \approx 0\%$).

However, the ¹³C NMR spectra become more complicated and gain sharper spectral features at extended ¹H DNP times, see Figures 3b and 3c. At ~30.6 mins, the ¹³C NMR spectra are comprised of (at least) two main resonances with differing NMR signal intensities. In the case of positive microwave irradiation (Figure 3b), the frequency separation between the two most intense ¹³C NMR peaks is ~8.4 kHz and the linewidth at FWHM is ~17.7 kHz. It is interesting to note that the ¹³C NMR spectra acquired in the cases of positive (Figure 3b) and negative (Figure 3c) microwave irradiation do not have the same overall profile at long ¹H DNP times. These spectra correspond to much higher levels of ¹H polarization ($|P_H| \ge 55\%$).

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.92Figure 3: Relevant portions of the experimental ¹³C NMR spectra belonging to the ¹³C-labelled methyl group (¹³CH₃) of [2-¹³C]sodium acetate acquired at.937.05 T (¹H nuclear Larmor frequency = 300.13 MHz, ¹³C nuclear Larmor frequency = 75.47 MHz) and 1.2 K with a single transient (*rf*-pulse flip angle =.943.5°) at two different ¹H DNP times. The labels indicate the ¹H DNP times at which the spectra were recorded. The timings coincide with those shown in.95Figure 2. The ¹³C NMR spectra were acquired by using the *rf*-pulse sequence depicted in Figure 1. (a) No microwave irradiation; (b) Positive microwave.96irradiation; and (c) Negative microwave irradiation. All ¹³C NMR spectra have been scaled to yield the same maximum intensity.

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.98 3.3. ¹³C NMR Peak Normalized Centre of Gravity Deviation vs. ¹H Polarization

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:00 The DNP build-up curve for the ¹H polarization $P_{\rm H}$ as a function of the ¹H DNP time for positive microwave irradiation is shown :01 in Figure 4. More details regarding how to acquire such build-up curves are given in the following reference (Elliott et al, 2021b). 202 The ¹H polarization build-up curve was found to have a stretched exponential behaviour, and the experimental data are well fitted with a stretched exponential function using a ¹H DNP build-up time constant denoted τ_{DNP}^+ . Stretched exponential function: A(1-:03 $\exp\{-(t/\tau_{DNP}^+)^{\beta}\})$, where A is a constant, τ_{DNP}^+ is the ¹H DNP build-up time constant extracted from the above fitting procedure 204 and β is the breadth of the distribution of ¹H DNP build-up time constants. The mean ¹H DNP build-up time constant $\langle \tau_{DNP}^+ \rangle$ is 205 calculated as follows: $\langle \tau_{DNP}^+ \rangle = \tau_{DNP}^+ \Gamma(1/\beta)/\beta$, where $\Gamma(1/\beta)$ is the gamma function. A similar ¹H polarization build-up curve :06 for the case of negative microwave irradiation, with parameters τ_{DNP} and $\langle \tau_{DNP} \rangle$, is shown in the Supplement. :07

The sample polarized to $P_{\rm H} \simeq -77.3\%$ (¹H DNP time $\simeq 30.6$ mins) by employing negative microwave irradiation with a ¹H DNP build-up time constant of $\langle \tau_{\rm DNP}^- \rangle = 122.0 \pm 0.4$ s ($\beta = 0.87$). A reduced ¹H polarization of $P_{\rm H} \simeq 58.1\%$ was reached (at ¹H DNP time $\simeq 30.6$ mins) by using positive microwave irradiation. The ¹H DNP build-up time constant was much shorter in this case: $\langle \tau_{\rm DNP}^+ \rangle = 80.2 \pm 0.3$ s ($\beta = 0.77$).

The ¹³C NMR lineshapes presented in Figure 3 are complicated and so it is desirable to construct a parameter which can describe the ¹H polarization $P_{\rm H}$, be robust with respect to field inhomogeneities and easily applied to any lineshape. Figure 4 therefore also displays the ¹³C NMR peak CoG deviation δ_{ω_0} as a function of the ¹H DNP time for the case of positive microwave irradiation. The ¹³C NMR peak CoG normalized deviation δ_{ω_0} is defined as:

$$17 \qquad \delta_{\omega_0} = \frac{M_{asym}}{LW_0} (1)$$

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 M_{asym} is denoted as the first moment of asymmetry and corresponds to the following quantity:

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$$M_{asym} = \int_{-\infty}^{\infty} (\omega - \omega_0 (P_H = 0\%)) f(\omega) \, d\omega \, (2)$$

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The first moment of asymmetry M_{asym} is based on a calculation whereby the CoG of the ¹³C NMR peak ω_0 is held constant at $\omega_0(P_H = 0\%)$, *i.e.*, the ¹³C NMR peak CoG corresponding to when the ¹H polarization P_H is zero. The CoG of the ¹³C NMR peak ω_0 is calculated as:

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$$27 \qquad \omega_0 = \int_{-\infty}^{\infty} \omega f(\omega) \, d\omega \, (3)$$

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 129 where the intensities of the 13 C NMR peaks are normalized:

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$$31 \quad \int_{-\infty}^{\infty} f(\omega) \ d\omega = 1 \ (4)$$

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where ω is the resonance frequency and $f(\omega)$ is the peak intensity at ω . The procedure outlined above ensures that $M_{asym} = 0$ at P_H = 0% such that the described approach can be readily generalized to any lineshape. The quantity LW_0 is a measure of the linewidth of the ¹³C NMR peak in the case of $P_{\rm H} = 0\%$:

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$$LW_0 = \sqrt{\int_{-\infty}^{\infty} (\omega(P_H = 0\%) - \omega_0(P_H = 0\%))^2 f(\omega(P_H = 0\%)) \, d\omega \, (5)}$$

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i.e., the square root of the second moment at $P_{\rm H} = 0\%$. This factor establishes a ¹³C NMR peak CoG deviation δ_{ω_0} (defined in Equation 1) which is a normalized and dimensionless quantity.

Figure 4 indicates that at longer ¹H DNP times, where the ¹H polarization $P_{\rm H}$ is higher, there is a greater ¹³C NMR peak CoG normalized deviation δ_{ω_0} . Similar curves to those presented in Figure 4 for the case of negative microwave irradiation are shown in the Supplement. It should be noted that the curve profiles and final values of δ_{ω_0} are not mirror images of each other. This is also reflected in the ¹³C NMR spectra acquired at ~30.6 mins, see Figure 3. The rate of change in the value of δ_{ω_0} during the first ~100 s of Figure 4 indicates a more rapid change in the ¹H polarization $P_{\rm H}$. This coincides with the starkest changes in ¹³C NMR lineshape, see the Supplement.





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Figure 4: Experimental ¹H polarization $P_{\rm H}$ DNP build-up curve (black filled squares and left-hand axis) and ¹³C NMR peak CoG normalized deviation δ_{ω_0} (grey empty circles and right-hand axis) as a function of the ¹H DNP time acquired at 7.05 T (¹H nuclear Larmor frequency = 300.13 MHz, ¹³C nuclear Larmor frequency = 75.47 MHz) and 1.2 K with a single transient per data point for the case of positive microwave irradiation. The timings coincide with those shown in Figure 2. The black solid line indicates the best fit of the experimental data points for the ¹H polarization $P_{\rm H}$ DNP build-up curve, and has the corresponding fitting function: A(1-exp{-(t/ $\tau_{\rm DNP}^{\pm})^{\beta}$). Mean ¹H DNP build-up time constant: $\langle \tau_{\rm DNP}^{+} \rangle = 80.2 \pm 0.3$ s.

The ¹³C NMR peak CoG normalized deviation δ_{ω_0} as a function of the ¹H polarization $P_{\rm H}$ for positive microwave irradiation is shown in Figure 5. The ¹H polarization $P_{\rm H}$ increases with an increasing ¹³C NMR peak CoG normalized deviation. The experimental data were fitted with a phenomenological relationship of the kind: $P_{\rm H}(\delta_{\omega_0}) = A \times \delta_{\omega_0}^{\beta}$, where $P_{\rm H}(\delta_{\omega_0})$ is the ¹H polarization as a function of the ¹³C NMR peak CoG normalized deviation δ_{ω_0} , β is the order of the polynomial fit and A is a scaling factor. The phenomenological function is simply used to correlate the ¹³C NMR peak CoG normalized deviation δ_{ω_0} with the ¹H polarization $P_{\rm H}$. The best fit values of the phenomenological function to the experimental data over the range of ¹³C NMR peak CoG normalized deviations shown in Figure 5 are given in the caption.

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Figure 5: Experimental ¹H polarizations $P_{\rm H}$ as a function of the ¹³C NMR peak CoG normalized deviation δ_{ω_0} acquired at 7.05 T (¹H nuclear Larmor frequency = 300.13 MHz, ¹³C nuclear Larmor frequency = 75.47 MHz) and 1.2 K with a single transient per data point for the case of positive microwave irradiation. The experimental data were fitted with a phenomenological function: $P_{\rm H}(\delta_{\omega_0}) = A \times \delta_{\omega_0}^{\beta}$. Best fit values: $A = 129.1\% \pm 0.8\%$; $\beta = 0.736 \pm$ 0.005. The absolute ¹H polarizations $P_{\rm H}$ were measured by comparison with a thermal equilibrium ¹H NMR signal.

271 4. Discussion

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As discussed in Section 3.3 above, the CoG normalized deviation δ_{ω_0} of the peaks in the ¹³C NMR spectrum indirectly provide the level of ¹H polarization $P_{\rm H}$, see Figure 5. It is unlikely that a uniform spin temperature between the ¹H and ¹³C nuclear spin reservoirs is reached at any time during the experiment presented in Figure 1, but as long as a uniform spin temperature is achieved within the ¹H nuclear spin reservoir then the methodology presented above holds. It should be noted that the order of the polynomial fit β shown in Figure 5 is likely to be influenced by the capabilities of the *rf*-probe, such as the *rf*-pulse homogeneity, and it is therefore recommended that (if possible) users implement similar measurements on their own experimental setups, rather than simply reusing the value presented here. In this way, any laboratory can adopt the procedure and reproduce the result.

:80 Once the ¹³C NMR peak CoG normalized deviation δ_{ω_0} falls below zero the ¹H polarization $P_{\rm H}$ rapidly drops towards negative values, see the Supplement. This result implies that the NMR peak CoG normalized deviation δ_{ω_0} is less sensitive to negative 281 microwave irradiation. This change in sensitivity of the 13 C NMR peak CoG normalized deviations δ_{ω_0} to positive and negative 82 microwave irradiation is also evident in the ¹³C NMR spectra, see Figure 3 and the Supplement. This is likely associated with: (i) :83 ¹³C NMR spectra at negative levels of ¹H polarization have lineshapes with less pronounced features, *i.e.*, partially unresolved 284 :85 peaks; and (ii) the ¹³C NMR lineshape changes less dramatically as a function of negative ¹H polarization. These points could both :86 be related to NMR line narrowing due to radiation damping for the case of negative microwave irradiation (Mao and Ye, 1997; :87 Krishnan and Murali, 2013).

¹H polarizations in the range of $0\% \leq P_{\rm H} \leq 30\%$ typically correspond to those accrued by ¹H DNP build-up experiments performed at liquid helium temperatures of 3.8-4.2 K. These results indicate that the ¹³C NMR peak CoG normalized deviation δ_{ω_0} can therefore also be used to infer ¹H polarizations $P_{\rm H}$ accurately at elevated temperatures. However, the presence of methyl group rotation at temperatures above 1.2 K is likely to somewhat average the ¹H-¹³C dipolar couplings and could lead to a different trend compared with the fit presented in Figure 5 (Latanowicz, 2005).

¹⁹³One possible contribution to the inflexion in the fit of the ¹³C NMR peak CoG normalized deviations δ_{ω_0} at low levels of ¹H ¹⁹⁴polarization $P_{\rm H}$ is the presence of strong polarization gradients or highly polarized clusters of nuclear spins located within specific ¹⁹⁵radii of the electron spins within the sample at short ¹H DNP times, which would lead to a non-uniform spin temperature. This ¹⁹⁶contribution is expected to be minor.

The decay of ¹³C polarization during the ¹H DNP build-up interval t_{DNP}^2 shown in Figure 2 occurs when the microwave source 297 is active and the ¹³C nuclear spin ensemble relaxes towards the spin temperature it would have achieved in the case of direct ¹³C :98 DNP, i.e., no CP. This ¹³C polarization decay is a combination of three factors: (i) the microwaves are active and hence polarization :99 is diminishing towards the low DNP equilibrium of the ¹³C nuclear spins with TEMPOL as the polarizing agent; (ii) the ¹³C nuclear :00 :01 spins are being actively pulsed, although minimally, every 5 s, which leads to an accumulative loss of ¹³C NMR signal intensity over many minutes; and (iii) the radical concentration and temperature are in an optimal range for thermal mixing (Guarin et al, :02 2017) and since the ¹³C spins are polarized whilst the ¹H spins are saturated the two nuclear pools most likely exchange energy via :03 the electron non-Zeeman reservoir, which influences the time evolution of the ¹³C magnetization until the ¹H spins achieve the :04 same spin temperature. The difference in the ¹³C polarizations $P_{\rm C}$ at ¹H DNP time = 24 mins for positive and negative microwave :05 irradiation is associated with the ¹H polarization build-ups and the performance efficiency of the multiple-contact CP rf-pulses, see :06 :07 the Supplement.

The ¹³C NMR lineshapes of $[2^{-13}C]$ sodium acetate shown in Figure 3 have features which mainly originate from ¹³C chemical shift anisotropy (CSA) (max. ~1.5 kHz at our magnetic field of 7.05 T) and ¹H-¹³C dipolar couplings (typ. -22.7 kHz) that are affected by possible methyl group rotation. Since the ¹³C CSA is negligible with respect to the ¹H-¹³C dipolar couplings, it is assumed that the ¹H-¹³C dipolar couplings play the key role in the ¹³C NMR lineshape of $[2^{-13}C]$ sodium acetate. The smaller ¹³C NMR peak contributions observed near the baseline in Figure 3a likely correspond to different chemical environments within the sample which are being polarized on different time scales.

- The values of δ_{ω_0} , $P_{\rm H}$ and the order of the polynomial fit β presented in Figure 5 are likely to depend to a small degree on the :14 solvent constituents. In the case of our sample, the glycerol- d_8 present in the dDNP glassing matrix yields an approximate ¹³C ;15 concentration of ~410 mM at natural abundance, which is ~14% of the total ¹³C spin concentration. Under microwave irradiation, :16 the natural abundance ¹³C spins of glycerol-d₈ will be polarized with their own build-up rate and maximum polarization, and :17 although deuterated glycerol- d_8 can also be polarized by ¹H-¹³C CP (Vuichoud et al, 2019). As such, these contributions could :18 ;19 impact the ¹³C NMR peak intensities, which would go some way to explaining why the ¹³C NMR spectra are not of the same overall profile under positive and negative microwave irradiation at long proton DNP times, see Figures 3b and 3c. It is also possible that :20 the dipolar couplings and CSA interactions manifest differently under positive and negative microwave irradiation, and that there :21 is a preferred energy state for coupling to positive and negative ¹H polarizations $P_{\rm H}$ leading to non-identical ¹³C NMR spectra. 22
- The NMR spectra presented in Figure 3 were acquired for the cases of high ¹³C SNRs, the largest of which is ca. 1244. In the :23 :24 event that CP cannot be (efficiently) implemented, and the acquired ¹³C NMR signal is weak, we anticipate that the method is robust with respect to a few kilohertz of line broadening, which can be used to improve the experimental SNR. The value of the :25 ¹³C NMR peak CoG normalized deviation δ_{ω_0} is, however, likely to be sensitive to changes in phase, and this should therefore be :26 :27 taken into account before comparing experimental results to any calibration curves similar to those presented in Figure 5. It is also possible that additional phase corrections may help the trend shown in Figure 5 move closer to a linear fit for values of $\delta_{\alpha \alpha} < 0.02$. 28 The results of this study suggest that other ¹³C-labelled molecules which might display distinct solid-state ¹³C NMR spectra, :29 such as $[1-^{13}C]$ sodium formate and other $^{13}CH_3$ (or $^{13}CH_2$) group bearing molecular candidates (presence of a strong $^{1}H^{-13}C$ dipolar 30 31 coupling), could also be used as indirect ¹H polarization meters (polarimeters). To effectively polarize both ¹H and ¹³C nuclear 32 spins, future experiments could use a tailored mixture of radical species, in certain cases. Clearly, at low levels of ¹H polarization 33 $P_{\rm H}$ the lower intensity resonance is unresolved and polluted by the more intense peak, and as such; the presented analysis could be
- further improved by considering Voigt fits of the complicated ¹³C NMR spectra, but since there are a number of resonances to consider this route would lead us away from our simple pedagogical approach.
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5 Conclusions

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We have demonstrated that ¹³C NMR lineshape polarimetry of [2-¹³C]sodium acetate can be implemented to indirectly infer the ¹H :39 polarization of the ¹³CH₃ group nuclear spins and potentially the whole sample if the constituents of which are sufficiently 40 homogeneously mixed. An easy to implement protocol based on the normalized deviation of the centre of gravity of the ¹³C NMR 41 peaks was employed and a simple relationship with ¹H polarization was found. This approach is complementary to traditional 42 methods of measuring ¹H polarization, in suitable circumstances, and could be useful in situations where measurements of ¹H 43 :44 polarizations prove difficult, e.g., due to radiation damping (Mao and Ye, 1997; Krishnan and Murali, 2013), which can also likely impact the experimental data and order of the polynomial fit shown in Figure 5. Other appropriate cases for potential :45 implementation include: (i) the lack of a ¹H rf-coil; (ii) the presence of large background signals; and (iii) the absence of a thermal 46 equilibrium spectrum. The approach presented here works well for traditional dDNP-compatible sample formulations but future ;47 studies employing fully deuterated dDNP solutions could provide ¹³C NMR lineshapes with more distinct features. 48

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Author Contributions

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SJE conceived the idea, performed experiments, processed the data and wrote the manuscript, QS assisted with experiments and data processing, and provided useful advice, and SJ provided informative guidance, supportive feedback and contributed to the manuscript.

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70 Data Availability

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Experimental data are available upon request from the corresponding author.

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Competing Interests

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The authors declare no competing interests.

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Ardenkjær-Larsen, J.-H., Fridlund, B., Gram, A., Hansson, G., Hansson, L., Lerche, M. H., Servin, R., Thaning, M., and Golman, K.: Increase in signal-to-noise
 ratio of > 10,000 times in liquid-state NMR, Proc. Natl. Acad. Sci. U.S.A., 100, 10158-10163, https://doi.org/10.1073/pnas.1733835100, 2003.

- 82 Hirsch, M. L., Kalechofsky, N., Belzer, A., Rosay, M., and Kempf, J. G.: Brute-Force Hyperpolarization for NMR and MRI, J. Am. Chem. Soc., 137, 8428-8434, 83 https://doi.org/10.1021/jacs.5b01252, 2015.
- 84 Dale, M. W., and Wedge, C. J.: Optically generated hyperpolarization for sensitivity enhancement in solution-state NMR spectroscopy, Chem. Commun., 52, 85 13221-13224, https://doi.org/10.1039/C6CC06651H, 2016.
- 86 Meier, B.: Quantum-rotor-induced polarization, Magn. Reson. Chem., 56, 610-618, https://doi.org/10.1002/mrc.4725, 2018.
- 87 Kouřil, K., Kouřilová, H., Bartram, S., Levitt, M. H., and Meier, B.: Scalable dissolution-dynamic nuclear polarization with rapid transfer of a polarized solid, Nat. 88 Commun., 10, 1733, https://doi.org/10.1038/s41467-019-09726-5, 2019.
- 89 Nelson, S. J., Kurhanewicz, J., Vigneron, D. B., Larson, P. E. Z., Harzstark, A. L., Ferrone, M., van Criekinge, M., Chang, J. W., Bok, R., Park, I., Reed, G.,
- :90 Carvajal, L., Small, E. J., Munster, P., Weinberg, V. K., Ardenkjær-Larsen, J.-H., Chen, A. P., Hurd, R. E., Odegardstuen, L.-I., Robb, F. J., Tropp, J., and Murray, ;91 J. A.: Metabolic imaging of patients with prostate cancer using hyperpolarized [1-13C]pyruvate, Sci. Trans. Med., 5, 198ra108, 92 https://doi.org/10.1126/scitranslmed.3006070, 2013.
- :93 Chen, H.-Y., Aggarwal, R., Bok, R. A., Ohliger, M. A., Zhu, Z., Lee, P., Goodman, J. W., van Criekinge, M., Carvajal, L., Slater, J. B., Larson, P. E. Z., Small, E. 94 J., Kurhanewicz, J. and Vigeron, D. B.: Hyperpolarized ¹³C-pyruvate MRI detects real-time metabolic flux in prostate cancer metastases to bone and liver: a clinical :95 feasibility study, Prostate Cancer Prostatic Dis., 23, 269-276, https://doi.org/10.1038/s41391-019-0180-z, 2020.
- :96 Gallagher, F. A., Woitek, R., McLean, M. A., Gill, A. B., Garcia, R. M., Provenzano, E., Reimer, F., Kaggie, J., Chhabra, A., Ursprung, S., Grist, J. T., Daniels, C.
- ;97 J., Zaccagna, F., Laurent, M.-C., Locke, M., Hilborne, S., Frary, A., Torheim, T., Boursnell, C., Schiller, A., Patterson, I., Slough, R., Carmo, B., Kane, J., Biggs,
- 98 H., Harrison, E., Deen, S. S., Patterson, A., Lanz, T., Kingsbury, Z., Ross, M., Basu, B., Baird, R., Lomas, D. J., Sala, E., Watson, J., Rueda, O. M., Chin, S.-P.,
- :99 Wilkinson, I. B., Graves, M. J., Abraham, J. E., Gilbert, F. J., Caidas, C., and Brindle, K. M.: Imaging breast cancer using hyperpolarized carbon-13 MRI, Proc. 00 Natl. Acad. Sci., 117, 2092-2098, https://doi.org/10.1073/pnas.1913841117, 2020.
- -01 Abragam, A., and Goldman, M.: Principles of dynamic nuclear polarisation., Rep. Prog. Phys., 41, 395-467, https://doi.org/10.1088/0034-4885/41/3/002, 1978.
- -02 Kundu, K., Mentink-Vigier, F., Feintuch, A., and Vega, S.: DNP mechanisms, eMagRes, 8, 295-338, https://doi.org/10.1002/9780470034590.emrstm1550, 2019.
- -03 Meier, B., Dumez, J.-N., Stevanato, G., Hill-Cousins, J. T., Roy, S. S., Håkansson, P., Mamone, S., Brown, R. C. D., Pileio, G., and Levitt, M. H.: Long-Lived
- 04 Nuclear Spin States in Methyl Groups and Quantum-Rotor-Induced Polarization, J. Am. Chem. Soc., 135, 18746-18749, https://doi.org/10.1021/ja410432f, 2013.
- -05 Roy, S. S., Dumez, J.-N., Stevanato, G., Meier, B., Hill-Cousins, J. T., Brown, R. C. D., Pileio, G., and Levitt, M. H.: Enhancement of quantum rotor NMR signals 06 by frequency-selective pulses, J. Magn. Reson., 250, 25-28, https://doi.org/10.1016/j.jmr.2014.11.004, 2015.
- 07 Dumez, J.-N., Vuichoud, B., Mammoli, D., Bornet, A., Pinon, A. C., Stevanato, G., Meier, B., Bodenhausen, G., Jannin, S., and Levitt, M. H.: Dynamic Nuclear
- -08 Polarization of Long-Lived Nuclear Spin States in Methyl Groups, J. Phys. Chem. Lett., 8, 3549-3555, https://doi.org/10.1021/acs.jpclett.7b01512, 2017.
- -09 Elliott, S. J., Meier, B., Vuichoud, B., Stevanato, G., Brown, L. J., Alonso-Valesueiro, J., Emsley, L., Jannin, S., and Levitt, M. H.: Hyperpolarized long-lived 10 nuclear spin states in monodeuterated methyl groups, Phys. Chem. Chem. Phys., 20, 9755-9759, https://doi.org/10.1039/C8CP00253C, 2018.
- 11 Waugh, J. S., Gonen, O., and Kuhns, P.: Fourier transform NMR at low temperatures, J. Chem. Phys., 86, 3816-3818, https://doi.org/10.1063/1.451940, 1987.
- Kuhns, P., Gonen, O., and Waugh, J. S.: Proton spin-spin and spin-lattice relaxation in CaSO4·xH2O below 1 K, J. Magn. Reson., 82, 231-237, 12 13 https://doi.org/10.1016/0022-2364(89)90027-9, 1989.
- 14 Marohn, J. A., Carson, P. J., Hwang, J. Y., Miller, M. A., Shykind, D. N., and Weitekamp, D. P.: Optical Larmor beat detection of high-resolution nuclear magnetic resonance in a semiconductor heterostructure., Phys. Rev. Lett., 75, 1364-1367, https://doi.org/10.1103/PhysRevLett.75.1364, 1995.
- 16 Kuzma, N. N., Håkansson, P., Pourfathi, M., Ghosh, R. K., Kara, H., Kadlecek, S. K., Pileio, G., Levitt, M. H., and Rizi, R. R.: Lineshape-based polarimetry of dynamically-polarized ¹⁵N₂O in solid-state mixtures, J. Magn. Reson., 234, 90-94, https://doi.org/10.1016/j.jmr.2013.06.008, 2013.
- 18 Mammoli, D., Salvi, N., Milani, J., Buratto, R., Bornet, A., Sehgal, A. A., Canet, E., Pelupessy, P., Carnevale, D., Jannin, S., and Bodenhausen, G.: Challenges in preparing, preserving and detecting para-water in bulk: overcoming proton exchange and other hurdles, Phys. Chem. Chem. Phys., 17, 26819-26827, 20 https://doi.org/10.1039/C5CP03350K, 2015.
- 21 Willmering, M. M., Ma, Z. L., Jenkins, M. A., Conley, J. F., and Hayes, S. E.: Enhanced NMR with Optical Pumping Yields ⁷⁵As Signals Selectively from a Buried 22 GaAs Interface, J. Am. Chem. Soc., 139, 3930-3933, https://doi.org/10.1021/jacs.6b08970, 2017.
- 23 Aghelnejad, B., Marhabaie, S., Baudin, M., Bodenhausen, G., and Carnevale, D.: Spin Thermometry: A Straightforward Measure of Millikelvin Deuterium Spin 24 Temperatures Achieved by Dynamic Nuclear Polarization, J. Phys. Chem. Lett., 11, 3219-3225, https://doi.org/10.1021/acs.jpclett.0c00713, 2020.
- 25 Elliott, S. J., Ceillier, M., Cala, O., Stern, Q., Cousin, S. F., El Daraï, T., and Jannin, S., In Preparation, 2021.
- 26 Bornet, A., Milani, J., Vuichoud, B., Perez Linde, A. J., Bodenhausen, G., and Jannin, S.: Microwave frequency modulation to enhance Dissolution Dynamic 27 Nuclear Polarization, Chem. Phys. Lett., 602, 63-67, https://doi.org/10.1016/j.cplett.2014.04.013, 2014.
- 28 Bornet, A., Pinon, A., Jhajharia, A., Baudin, M., Ji, X., Emsley, L., Bodenhausen, G., Ardenkjær-Larsen, J.-H., and Jannin, S.: Microwave-gated dynamic nuclear 29 polarization, Phys. Chem. Chem. Phys., 18, 30530-30535, https://doi.org/10.1039/C6CP05587G, 2016.
- 30 Cheng, T., Capozzi, A., Takado, Y., Balzan, R., and Comment, A.: Over 35% liquid-state ¹³C polarization obtained via dissolution dynamic nuclear polarization at 31 7 T and 1 K using ubiquitous nitroxyl radicals: Phys. Chem. Chem. Phys, 15, 48, https://doi.org/10.1039/C3CP53022A, 2013.
- 32 Elliott, S. J., Stern, Q., Ceillier, M., El Daraï, T., Cousin, S. F., Cala, O., and Jannin, S.: Practical Dissolution Dynamic Nuclear Polarization, Accepted in Prog. 33 Nucl. Magn. Reson. Spectrosc., https://doi.org/10.1016/j.pnmrs.2021.04.002, 2021.

- 15
- 17
- 19

- Mao, X. A., and Ye, C. H.: Understanding radiation damping in a simple way, Concepts Magn. Reson. A, 9, 173-187, https://doi.org/10.1002/(SICI)1099-
- **\35** 0534(1997)9:3<173::AID-CMR4>3.0.CO;2-W, 1997.
- 36 Krishnan, V. V., and Murali, N.: Radiation damping in modern NMR experiments: Progress and challenges, Prog. Nucl. Magn. Reson. Spectrosc., 68, 41-57,
- **\37** https://doi.org/10.1016/j.pnmrs.2012.06.001, 2013.
- Latanowicz, L.: NMR relaxation study of methyl groups in solids from low to high temperatures, Concept Magn. Reson. A, 27A, 38-53,
 https://doi.org/10.1002/cmr.a.20040, 2005.
- 40 Guarin, D., Marhabaie, S., Rosso, A., Abergel, D., Bodenhausen, G., Ivanov, K. L., and Kurzbach, D.: Characterizing Thermal Mixing Dynamic Nuclear
- 41 Polarization via Cross-Talk between Spin Reservoirs, J. Phys. Chem. Lett., 8, 5531-5536, https://doi.org/10.1021/acs.jpclett.7b02233, 2017.
- 42 Vuichoud, B., Milani, J., Bornet, A., Melzi, R., Jannin, S., and Bodenhausen, G.: Hyperpolarization of Deuterated Metabolites via Remote Cross-Polarization and
- Dissolution Dynamic Nuclear Polarization, J. Phys. Chem. B, 118, 1411-1415, https://doi.org/10.1021/jp4118776, 2014.