



1 When the MOUSE leaves the house

- 2 Bernhard Blümich¹, Jens Anders²
- 3 ¹Independent researcher, 52159 Roetgen, Germany
- 4 ²Institute of Smart Sensors, University of Stuttgart, 70569 Stuttgart, Germany
- 5 Correspondence to: Bernhard Blümich (<u>bluemich@rwth-aachen.de</u>)

Abstract. Change is inherent to time being transient. With the NMR-MOUSE having matured into an established
NMR tool for nondestructive testing of materials, this forward-looking retrospective assesses the challenges the
NMR-MOUSE faced when deployed outside a protected laboratory and how it's performance quality can be
maintained and improved when operated under adverse conditions in foreign environments. This work is dedicated
to my dear colleague and friend Geoffrey Bodenhausen on the occasion of his crossing an honorable timeline in
appreciation of his ever-continuing success of fueling the dynamics of magnetic resonance.

12 1. Introduction

13 The MOUSE (MObile Universal Surface Explorer) (Eidmann et al., 1996) is a portable stray-field NMR sensor 14 suited for non-destructive testing of materials (Blümich et al., 2008; Casanova et al., 2011) With it the relaxation 15 of nuclear spins towards equilibrium is measured following perturbation by radio-frequency pulses. The sensor is 16 a small and compact NMR relaxometer that investigates an object from one side and can be carried along to the 17 site of interest. As such the NMR-MOUSE and other stray field relaxometers are one modality of compact NMR. 18 Other modalities are tabletop relaxometers, tabletop imagers and tabletop spectrometers (Blümich et al., 2014; 19 Blümich, 2016; Blümich and Singh, 2018).

20 While the size of most NMR instruments today is dominated by a large superconducting magnet, compact 21 NMR relaxometers have small permanent magnets. They were commercially introduced in the early 1970ies to 22 assist the food industry in characterizing emulsions (van Putte and van den Enden, 1974; Blümich, 2019). Today 23 tabletop relaxometers are employed to study a wide range of materials, in particular, foodstuffs, polymers, and 24 porous media (Blümich et al., 2014; Blümich, 2016; Blümich and Singh, 2018; Saalwächter, 2012). A key feature 25 of these early tabletop instruments is that samples need to be drawn and inserted into the hole in the magnet for 26 analysis. In this respect, the measurement is destructive. This equally applies to modern tabletop NMR 27 spectrometers for chemical analysis unless they are operated in flow-through mode, like in a process control 28 environment (Kern et al., 2019). While NMR spectrometers with permanent magnets were built already in the 29 early 1950s (Gutowski, 1953; Blümich, 2019), their magnets were large and could produce only a small field 30 region sufficiently homogeneous to resolve the proton chemical shift. Small permanent magnets with 31 homogeneous fields are challenging to build due to the variations in dimensions, polarization magnitude, and 32 direction of the magnet elements. Therefore, the routine use of compact NMR instruments remained limited for a 33 long time to relaxation and diffusion measurements until the technology of compact high-resolution magnets had 34 been sufficiently advanced about ten years ago (Danieli et al., 2010; Blümich, 2016; Blümich and Singh, 2018). 35 Before that, chemical analysis with tabletop instruments was explored primarily by a few dedicated research 36 groups (Nordon et al., 2001; Dalitz et al., 2012).





37 Mobile NMR instruments need to be both compact and robust to deploy them at different sites and in 38 different environments. The era of mobile NMR began with well-logging instruments shortly after the first NMR 39 experiments in condensed matter in December 1945. Already in 1952, Russel Varian patented a subsurface well 40 logging method and apparatus (Varian, 1952; Woessner, 2001). The sensor to be inserted into the borehole of an 41 oil-well and operating in the earth's magnetic field eventually evolved into tube-shaped instruments housing 42 permanent magnets as well as transmit and receive electronics to analyze the relaxation of ¹H NMR signals from 43 particular regions localized in the borehole wall (Jackson et al., 1980; Kleinberg and Jackson, 2001). In his 44 introduction to the 2016 book "Mobile NMR and MRI" (Johns et al., 2016), Eiichi Fukushima reviews the 45 evolution of earth-field and mobile NMR with particular attention to these early developments (Fukushima, 2016). 46 Well-logging NMR is also known as inside-out NMR because the instrument is inserted into the object and 47 not the object into the magnet. Inside-out NMR is mobile but also destructive, as a hole needs to be drilled into the 48 object (Jackson et al., 1980, Coates et al., 1999). The underlying concept of mobile stray-field relaxometry was 49 extended at the Southwest Research Institute, San Antonio, Texas, to nondestructive materials testing with NMR 50 relaxometers accessing the object from one side. These instruments were already transportable, whereby some of 51 them using bulky and massive electromagnets, others more compact permanent magnets (Fukushima, 2016). The 52 magnets were laid out to maximize the field volume containing the spins which can be excited selectively from 53 within the bulk with rf pulses in an effort to maximize the hydrogen signal from the object of interest next to the 54 sensor deriving from moisture in soil, bridge decks, building structures, and food products (Fukushima, 2016; 55 Blümich et al., 2008; Blümich, 2016; Blümich, 2019). Within this volume the field gradient must be small so that the resonance frequencies of the spins inside are within the bandwidth of the rf excitation pulses. As a consequence, 56 57 the field strength was low.

58 One may argue that the era of mobile NMR with compact sensors essentially started with the appearance 59 of the NMR-MOUSE, a stray-field relaxometer that in its design disregarded the quest for a large sensitive volume 59 by fortuitous ignorance (Eidmann et al., 1996). The small sensor exhibits a large field gradient, and consequently 60 a small sensitive volume yet a strong stray field. Compared to larger sensors the opposing impacts on the sensitivity 61 a smaller signal-bearing volume and higher field strength turned out to largely balance each other so that at 63 comparable sensitivity the more compact sensors (Blümich et al., 2008) were easier to carry along and be moved 64 from one place to another than other stray-field sensors.

65 2. The NMR-MOUSE in the house

66 While brainstorming the simplest realization of NMR in 1993 at the Max-Planck Institute for Polymer Research 67 in Mainz, Peter Blümler asked the question: "Would it not be nice to have an NMR scanner that one moves across 68 the surface of an object to look inside just like an ultrasound scanner?" (Armstrong-Smith, 2015). The next day he 69 came with a drawing how such a device could look like, and we dubbed it NMR-MOUSE for 'MObile Universal 70 Surface Explorer'. Having taken up the Chair of Macromolecular Chemistry at RWTH Aachen University the 71 same year, the realization of the NMR-MOUSE was the project of Blümich's first PhD student Gunnar Eidmann, 72 who succeeded to get the first signal in 1995 (Eidmann et al., 1996). Hardware improvements, measurement 73 methodology and applications of the NMR-MOUSE were systematically explored over the years in particular by 74 Peter Blümler, Gisela Guthausen, Sophia Anferova, Valdimir Anferov, Federico Casanova and Juan Perlo. The 75 NMR-MOUSE has found numerous applications for nondestructive materials characterization by relaxation and

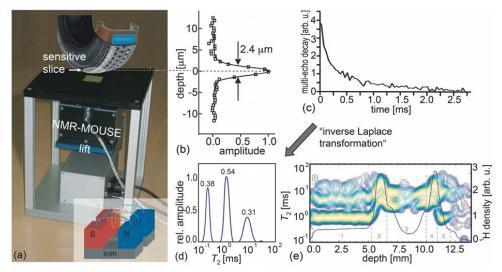




diffusion measurements (Blümich et al., 2008; Casanova et al., 2011). The design of many early stray-field relaxometers and of the original NMR-MOUSE was that of a simple u-shaped magnet. It is marketed by Bruker under the name 'minispec ProFiler'. This sensor has a roughly cup-shaped sensitive volume, the position, and shape of which are defined by the profiles of the stray fields produced by the permanent magnet and the radiofrequency coil (Eidmann et al., 1996, Hürlimann and Griffin, 2000; Balibanu et al., 2000).

81 A major improvement of the original sensor was to shim the sensitive volume from bowl-shape to a flat 82 with a slice diameter of about 10 mm, and, depending on the measurement scheme, a slice width less than 3 µm 83 (Perlo et al., 2005), enabling the acquisition of high-resolution depth profiles by translating the sensor in-between 84 measurements with high precision. To this end, two u-shaped or horseshoe magnets are placed side by side with a 85 small gap (Fig. 1a, bottom). The measurement principle followed to acquire depth profiles is the same as that 86 employed for logging oil wells except that the NMR-MOUSE sensor is horizontally moved between consecutive 87 measurements in steps on the order of 0.1 mm instead acquiring NMR signal while the well-logging tool is moving 88 laterally with respect to the magnet surface for distances on the order meters. Today, the NMR-MOUSE for high-89 resolution depth profiling is a heritage product of Magritek GmbH with its production site in Aachen, that is 90 managed by the two NMR-MOUSE pioneers Federico Casanova and Juan Perlo. In fact, Magritek today is the 91 result of a 2012 merger of Magritek Ltd. from New Zealand, which, among others, developed the Kea spectrometer 92 motivated by Paul Callaghan's Antarctic expeditions (Callaghan et al., 1998), and ACT GmbH, a company spun 93 off from RWTH Aachen University, which produced the Profile NMR-MOUSE.

94



95

Figure 1. The principle of measuring depth profiles with the Profile NMR-MOUSE. a) Conceptual picture of the profile NMR-MOUSE on a lift with its sensitive slice inside a rubber tire. b) Point-spread function of the record depth resolution. c) Experimental signal decay measured with a multi-echo train. d) Distribution of relaxation times from tire-tread rubber derived by inversion of a signal decay with an algorithm, referred to as "inverse Laplace transformation". e) Collection of distributions of relaxation times and signal amplitudes reporting nominal spin density measured across a range of 14 mm into a tire tread.

102

To measure depth profiles, the sensor is mounted on a precision displacement stage with which the sensitive
 slice at a fixed distance from the magnet surface can be moved through the object step by step between acquisitions
 of multi-echo trains and more advanced two-dimensional Laplace methods (Blümich et al., 2014). The envelope





106 of a multi-echo train provides a stroboscopically sampled transverse relaxation decay (Fig. 1c) from which a depth-107 profile amplitude can be derived in different ways to provide NMR parameter contrast based the relaxation-time 108 distribution (Fig. 1d), the hydrogen density corresponding to the signal amplitude from the spins in the sensitive 109 slice (Fig. 1e), relaxation times, and molecular self-diffusion (Blümich et al., 2008; Casanova et al., 2011; Blümich 110 et al., 2014). The signal amplitude is the full integral of the relaxation-time distribution. Partial integrals of 111 individual peaks provide component concentrations. To assign physical meaning to individual peaks is not as 112 straight forward as interpreting the chemical shift of resonance lines in a high-resolution NMR spectrum. Yet the 113 peak amplitudes and positions vary with material properties (Fig. 1e), and it often takes the treasure of experience 114 or a reference data base to interpret distributions of relaxation times for practical applications.

115



116

117 Figure 2. The evolution of stray-field NMR at RWTH Aachen University. a) The original NMR-MOUSE 118 measuring a car tire. b) An early version of the NMR-MOUSE with copper-shielded magnets for dead-time 119 reduction. c) The original NMR-MOUSE in 2000. d) The bar-magnet NMR-MOUSE is the simplest construction 120 of a stray-field NMR sensor. e) In 2003 Juan Perlo developed the smallest tomograph in stray-field technology 121 (Foto: Peter Winandy). f) A single-sided tomograph with a flat imaging plane. Right: Set-up for mapping a tire 122 tread. Left: A photo (top) in comparison with an MR image (bottom). g) The Profile NMR-MOUSE with a flat 123 sensitive slice developed in 2005. h) Stray-field NMR magnet capable of measuring chemical-shift resolved ¹H 124 NMR spectra from a fluid in a beaker placed on top of the magnet. i) Fourier NMR-MOUSE with shim magnets 125 producing a 2 mm thick sensitive slice for frequency encoding of depth. j) Mini-MOUSE with a multi-layered 126 micro-coil having a dead-time of 10 µs. k) Micro-MOUSE constructed from four 1 cm³ permanent magnet cubes. 127

128 The hardware, use, and measurement methodology of the NMR-MOUSE has been studied for more than 129 two decades in various research projects at RWTH Aachen University and other places. Its use for testing different 130 materials such as rubber, polymers, building materials, food, and objects of cultural heritage is reported in books 131 and reviews (Blümich, 2000; Blümich, 2008; Blümich et al., 2008; Blümich et al., 2010; Casanova et al., 2011; 132 Capitani et al., 2012; Blümich et al., 2014, Baias and Blümich, 2017; Capitani et al., 2017, Blümich, 2019; Rehorn 133 and Blümich, 2018; Blümich, 2019). Several modifications of the original NMR-MOUSE in addition to the





134 forerunner of the current Magritek Profile NMR-MOUSE (Fig. 1a) have been investigated at RWTH Aachen 135 University. Recognizing that the information content extractable from the signal of the sensitive region in stray-136 field NMR corresponds to that accessible in a voxel of a magnetic resonance image, first applications of the NMR-137 MOUSE were explored with car tires representing soft synthetic matter (Fig. 2a) in line with the main use of MRI 138 in imaging soft biological matter. The horseshoe set-up (Fig. 2b) was subsequently made smaller and packed in a 139 more attractive shell (Fig. 2c). Realizing that the horse-shoe magnet having the B_0 stray field essentially parallel 140 to its active surface could further be simplified, the bar-magnet NMR-MOUSE was built from a magnet block first 141 cuboid-shaped (Blümich et al., 2002) and later cylinder-shaped with B_0 perpendicular to the active end face and a 142 figure-eight rf coil with B_1 parallel to it (Fig. 2d). The maximum depth of access is lower than for the horseshoe 143 sensor, but the deadtime is shorter due to the gradiometer property of the rf coil (Anferova et al., 2002). Note that 144 contrary to the B_0 orientation perpendicular to the active surface, B_0 parallel to the active surface enables studying 145 macroscopic molecular order in anisotropic materials such as tendon and strained rubber (Haken and Blümich, 146 2000; Hailu et al, 2002.

147 While improving the original NMR-MOUSE, also a single-sided tomograph was developed and tested in 148 the DFG-funded Collaborative Research Center on Surface NMR of Elastomers and Biological Tissue FOR333. 149 One result from this project was the smallest MRI instrument at the time obtained by fitting a bar-magnet NMR-150 MOUSE with coils for pulsed gradient fields (Fig. 2e) (Casanova and Blümich, 2003). Another result was an 151 improved u-shaped magnet with thicker ends at each side of the poles so that the magnet assembly produced a flat 152 imaging plane (Fig. 2f) (Casanova and Blümich, 2003; Blümich et al., 2005). Images from a plane parallel to the 153 sensor surface could be measured with pure phase encoding schemes, but the sensitivity was low due to the thin 154 slice resulting from a strong stray-field gradient. Maintaining the flat sensitive region of the imaging plane, this 155 complex magnet geometry was subsequently simplified to two u-shaped magnets placed at a specific distance next 156 to each other, resulting in the Profile NMR-MOUSE (Fig. 1a, Fig. 2g), which proved to be a robust stray-field 157 NMR sensor constructed from a minimum number of parts (Perlo et al., 2005).

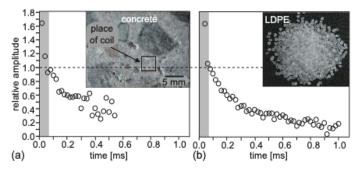
158 Flattening the sensitive region of a stray-field magnet to a plane was a milestone in understanding how to 159 shim the stray field. Eventually, the sensitive region in the stray field could be homogenized locally with the help 160 of additional shim magnets to a degree sufficient to resolve the ¹H chemical shift from a limited volume of fluid 161 inside a beaker on top of the magnet (Fig. 2h) (2014; Perlo et al., 2005; Perlo et al., 2006; Zalesskiy et al.). Another 162 advance was the construction of a stray-field sensor with a sensitive slice having a homogeneous gradient field in 163 the sensitive slice across an extended depth range of 2 mm for single-shot depth profiling by frequency encoding 164 of position (Fig. 2i) (Van Landeghem et al., 2012). With this sensor the time to acquire a depth profile into soft 165 matter was reduced considerably, and it proved useful for in vivo applications like mapping human skin [46] and 166 monitoring perfusion states of the small intestine by diffusion maps (Krechenau et al., 2018).

167 The NMR-MOUSE has also been miniaturized and fitted with multi-layered micro-coils (Fig. 2j,k) 168 (Oligschläger et al., 2014; Oligschläger, Kupferschläger, et al. 2015), by which, on the expense of 7.6-fold lower 169 sensitivity compared to the PM5 NMR-MOUSE at 1 mm access depth, the dead time of the measurement could 170 be reduced to a record 10 µs echo time. With its small coil, the signal from the cement regions between the stone 171 aggregate in cuts of concrete could be focused on, and with an echo time $\leq 20 \ \mu s$ the hitherto hidden signals from 172 bound water in the dry grey cement could be measured (Fig. 3a) (Oligschläger, Kupferschläger, et al. 2015). At 173 the same echo time, even the rapidly relaxing transverse magnetization from the crystalline domains of 174 polyethylene was detectable (Fig. 3b). The presence of the rapidly decaying signal components at $t_E = 20 \mu s$ nearly





175 doubles the amplitude of the recorded magnetization decays compared to the amplitudes recorded with the 176 minimum echo time of 70 µs of the reference laboratory NMR-MOUSE with 10 mm depth of access. As the short 177 dead time of the mini-MOUSE had been achieved at the cost of a small sensitive volume and a low depth of access 178 due to the small diameter of the coil, it is the ambition of current sensor improvement to reduce the deadtime at 179 coil diameters 10 mm and more. Currently, for example, the minimum echo time of the Magritek PM25 NMR-MOUSE is 50 µs when fitted with spacers and a 15 mm diameter coil to limit the depth of access to 10 mm. For a 180 181 new PM2 NMR-MOUSE with 2 mm depth of access the minimum echo time of the is just 15 µs. Even shorter 182 echo times may eventually be realized with novel transceiver circuits that promise the detection of the spin 183 response during the rf pulse (Anders, 2020). Moreover, to shorten the acquisition time from hours to minutes for 184 field applications like investigations of glass- or carbon-fiber reinforced polymer materials employed in windmill 185 wings and airplane rudders, the detection of the bitumen component in asphalt (Blümich et al., 2019) and the bound 186 water in cement, a large sensitive volume is needed. This can be achieved, for example, with a coil array 187 (Oligschläger, Lehmkuhl, et al. 2015) [53] placed on a suitably tailored magnet surface (Blümich et al., 1999). 188



189

Figure 3. Transverse magnetization decays acquired with the Mini-MOUSE (Fig. 2j) at short echo time t_E . The shaded area marks signal lost at a deadtime of 70 μ s. a) The signal from bound water in dry, grey cement. b) The

192 crystalline protons in low-density polyethylene with $T_2 = 12 \ \mu s$ can be detected at $t_E = 20 \ \mu s$.

193 3. The NMR-MOUSE outside the house

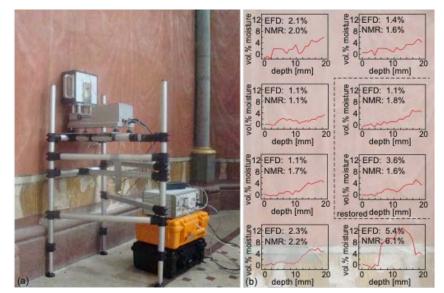
194 The NMR-MOUSE was introduced to the cultural heritage community through the effort of Annalaura Segre at 195 the turn of the millennium (Segre and Blümich, 2002), and from 1999 to 2019 its further refinement has benefitted 196 greatly from the cultural heritage projects EUREKA-Eurocare 212212-MOUSE, EU-ARTECH, CHARISMA, and 197 IPERION-CH. With the exception of well-logging relaxometry (Coates et al, 1999), it is common practice to 198 conduct NMR measurements in a laboratory. But objects of cultural heritage often cannot leave the museum or 199 are immobilized, e. g. at excavation sites, so that the NMR-MOUSE has to be moved to the site and operated under 200 the prevailing environmental and climatic conditions. These can be rather challenging at times for the operators as 201 well as for the equipment, which has been designed primarily for indoor use.

For some outdoor applications like determining the crumb-rubber content in asphalt pavements (Blümich
et al., 2019), depth profiling is not essential. But for others it is crucial. This includes the analysis of easel paintings
(Presciutti et al., 2008; Fife et al., 2015; Angelova et al., 2016; Prati et al., 2019; Busse et al., 2020), frescoes
(Rehorn et al., 2018), and mummies (Rühli et al., 2007; Blümich et al., 2014). A less obvious application is the
analysis of moisture distributions, for example, in walls. Moisture maps with crude lateral resolution and high





207 depth resolution can assist in locating a moisture leak (Proietti et al., 2007; Rehorn and Blümich, 2018; Blümich, 208 2019; Blümich in Bastidas and Cano, 2019). Although time consuming, high-resolution depth profiles of 209 volumetric, quantitative moisture content are more significant than the volume-averaged numbers delivered by 210 most methods other than the NMR-MOUSE including evanescent field dielectrometry (Olmi et al., 2006). The 211 latter method derives moisture content and the presence of salt from the dielectric properties of a wall exposed to 212 an electric field with a frequency of about 1 GHz. The electric wave enters the wall up to about 20 mm, so that the 213 delivered moisture content is a weighted volume average across that depth range. While the measurement is fast, 214 the depth resolution is inadequate for further analysis, because the moisture content varies significantly over the 215 20 mm as demonstrated with measurements of wall moisture in the Chapel of St. Mary of the Abbeye de Chaalis 216 (Fig. 4). Volumetric moisture content is easy to quantify at short echo time, by simply taking the signal amplitude 217 from a particular spot inside the wall and normalizing it to the amplitude of the signal from pure water measured 218 with the same instrumental parameter settings. 219



220

Figure 4. Moisture measurements at the painted wall left of the altar inside the Chapel of St. Mary in Chaalis. a) Set-up for NMR depth profiling. b) High-resolution depth profiles from eight positions. The moisture-content values from evanescent field dielectrometry (EFD) are compared to NMR values derived from integration of quantitative moisture depth profiles weighted with the heuristic depth attenuation function, which is indicated by the shaded region in the bottom left profile.

226

227 The measurement conditions encountered in historic buildings and outdoors are often challenging to meet 228 with equipment designed for laboratory use (Fig. 5). Examples are the presence of water, rain or steam (Fig. 229 5a,g,h), passing cars (Fig. 5b,c), testing spots a few meters high (Fig. 5d,e), and treasures of outstanding value 230 inside a guarded museum laboratory (Fig. 5f). The climate conditions can range from hot, e.g., up to 38° C air 231 temperature (Fig. 5c) and close to boiling water temperature (Fig. 5h) to cold, e.g. down to 5° C (Fig. 5a). The 232 environment may be dusty with magnetic sand particles or wet from streaming rain (Fig. 5g). In many cases, a 233 power grid can be accessed, but in some cases, the equipment needs to be operated from a battery (Fig. 6h) or an 234 electric power generator. Apart from the power supply, different units need to be connected with several cables at





235 the site. These units are an NMR-MOUSE with 10 mm or 25 mm depth range, a precision translational stage, a 236 fragile spectrometer console, and a laptop computer. The electrical connectors can break during transport and 237 assembly. The connecting cables often form ground loops that produce 50/60 Hz hum and pick up environmental 238 electromagnetic noise. However, the latter can successfully be shielded in most cases with the help of silver-coated 239 and electrically grounded parachute silk (Fig. 5g) or rabbit fence. Moreover, a stable scaffold finely adjustable in 240 height and suitable to be set up on uneven ground is needed to accurately position the NMR-MOUSE at the spot 241 of interest (Fig. 4a). All these parts along with basic tools for emergency repair are usually packed into plastic 242 transportation boxes and shipped to the site of interest prior to the measurement campaign.

243



244

Figure 5. The MOUSE outside the house. a) Profiling the moisture content of the grey concrete wall of the lock
Hohenwarthe. b) Profiling moisture in the concrete wall of the Gäubahn tunnel near Stuttgart. c) Analyzing the
crumb-rubber content in asphalt pavement (Foto: Yadoallah Teymouri). d) Assessing the fire damage of sandstone
in the Mackintosh library of Glasgow. e) Searching for a hidden Giotto fresco in Padua. f) Measuring a depth
profile though the back of a Stradivari violin in Cremona. g) In search for a hidden wall painting in Ostia Antica
on a rainy day. h) Profiling sediment-covered biofilms at the hot springs in Yellowstone National Park.

251

252 A practical point of concern in measuring high-resolution depth profiles is the proper placement of the 253 sensitive slice parallel to the stratigraphy of the object. Assuming that the sensitive slice is 10 mm wide and 0.1 254 mm thick, the misalignment angle between the plane of the slice and the layers to be resolved needs to be smaller 255 than one degree (Blümich et al., 2020). With a laboratory setup, the sensitive slice and the object surface can be 256 accurately aligned when the NMR-MOUSE is properly placed on the sample table of the lift to which the sensitive 257 slice had been aligned by the manufacturer (Fig. 1a). But measurements in the field usually employ a translation 258 stage without a sample table (Figs. 4a, 5f, 5h) so that the sensor is aligned with the object surface by eye. Moreover, 259 the minimum distance between the sensor and the object needs to be as small as possible, i. e. 1 mm or less, at the 260 start of profiling in order to maximize the depth range into the object. Setting alignment and minimum distance is





261 a critical part of the experiment setup. Electronic guidance for both would greatly simplify the setup procedure

and improve the reproducibility of measurement.

263 4. Improving the fitness of the NMR-MOUSE for adventures outside the house

- It is the accumulated experience with cultural heritage studies, which suggests a number of improvements to bring
 the NMR-MOUSE in shape for the adventures encountered when leaving the house and operating outdoors. These
 are:
- 267 1) Combine all electronics into one instrument comprising the translation stage, the NMR-MOUSE and the268 transmit-receive electronics.
- 269 2) Incorporate distance and alignment sensors into the instrument.
- 270 3) Employ a stable sensor scaffold and mounting device that can be assembled quickly at the site and enables
 271 measurements at different heights.
- 272
- power cable (a) (b) 25 from surface 22 15 MHz 20 20 distance 15 15 -10 0 z [mm] 10 -10 0 x [mm] 10 (d) (c

273

Figure 6. Concept of an all-in-one NMR-MOUSE for depth profiling. a) Axial cross section through two telescoped
tubes showing the stepper motor along with the transmit-receive electronics on the left in the outer tube and the
NMR-MOUSE on the right in the inner tube. b) Arrangement of magnets and alignment sensors. c) The instrument
should be controlled via WLAN or Bluetooth. d) Calculated field map predicting the position of the sensitive slice
at 22 mm above the magnet surface.

279 4.1 The all-in-one instrument

280 The envisioned all-in-one NMR-MOUSE for depth profiling outdoors would have a minimum number of 281 components connected by cables (Fig. 6). The components need to be small for ease of transportation and rugged 282 for operation outdoors. The power supply would be either a 12 V car battery or a power supply that connects to 283 the grid or an electric generator. It hooks up to the NMR instruments (Fig. 6a) with the only cable of the setup. 284 The instrument comprises the translation stage, the transmit-receive electronics, and the magnet (Fig. 6b). It would 285 be operated in wireless mode via WLAN or Bluetooth from a tablet personal computer (Fig. 6c), so that it can be 286 set up on tall scaffolds (Fig. 5e), and long measurements could be controlled and monitored from the distance 287 including the hotel room at night. 288 Assuming a 250 mm inner diameter tube, a computer simulation suggests that a Profile NMR-MOUSE

289 magnet configuration would produce a sensitive slice 22 mm above the magnet surface (Fig. 6d) with a field





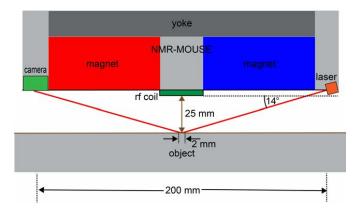
290 strength corresponding to a 15 MHz ¹H resonance frequency. Subtracting the space for the coil and the case, the 291 resultant depth of access would be 15 mm, which is a reasonable working depth for many applications ranging 292 from easel paintings to violins and frescoes. The magnets would be mounted in the inner of two telescoped tubes, 293 which can slide in and out of the outer one under control of a precision stepper motor. The outer tube would house 294 the stepper motor and the transmit-receive electronics and be attached to the mounting gear for depth profiling. 295 The total length of the pipe assembly would be shorter than 300 mm.

296 Commercial tabletop NMR instruments employ compact transmit-receive electronics (Blümich et al., 2014; 297 Blümich, 2016; Blümich and Singh, 2018), which, although reliable, nevertheless, are too large and power-hungry 298 for mobile use. Their state-of-the-art has been surpassed by the development of smaller, single-chip based 299 magnetic resonance transceivers (Zalesskiy et al., 2014; Ha et al., 2014; Ha et al., 2015; Grisi et al., 2015; Chu et 300 al., 2017; Anders et al., 2017). In particular, a small monolithic spectrometer has been developed (Bürkle et al., 2020), which uses a high-voltage CMOS process with supply voltages up to 25 V for enhanced driving strength to 301 302 combine the monolithic NMR-on-a-chip approach with macroscopic, cm-sized coils. This approach promises a 303 90°-pulse width of 5 µs for an echo time of 20 µs at a depth of access of 10 mm, rendering high-voltage NMR-on-304 a-chip transceivers well suited for use in a compact all-in-one NMR-MOUSE sensor.

305 4.2 Distance and alignment sensors

306 The implementation of distance and alignment sensors is a highly needed improvement over the current state-of-307 the-art, where the NMR sensor has to be aligned visually parallel to the object as close as 0.5 mm (Blümich et al., 308 2020). The misalignment angle of the sensitive slice with the parallel layer structures of the object needs to be less 309 than one degree if the spatial resolution is to be better than 200 µm. But visual alignment parallel to an extended 310 surface is hardly possible as one cannot see by eye the narrow gap between the magnet and the surface. 311 Nevertheless, in practice, object and sensor have usually been aligned visually (Fig. 5f,h) with surprisingly good 312 results in most cases but only fair reproducibility even for expert users. To enable the required reproducibility, 313 alignment sensors need to be incorporated with the help of which the sensitive plane can be accurately aligned 314 with the object at a fixed distance. Once aligned at a known distance, the sensor can be advanced or retracted to 315 its starting position with the stepper motor.

316



317

318 Figure 7. Concept of distance sensing with a laser beam at shallow incidence. If the alignment angle of the **319** reflecting plane changes by 0.2°, the reflected laser beam is displaced from the center of the detector camera by 4

10

319 refle 320 mm.





321

322 Elements for alignment-sensor components can be mounted in the four spaces of the inner tube delineated 323 by the tube's inner surface and the secants defined by the outer magnet surfaces (Fig. 5b). Different sensing 324 principles can be considered. The surface spot to align the sensor with the object needs to be at least one millimeter 325 wide to average effects of surface roughness. Therefore, ultrasonic distance sensors appear to be more suitable 326 than regular laser-point distance sensors with spot widths of 10 mm vs. 70 µm, respectively. Yet commercial 327 ultrasonic sensors measure distances within a 25 mm range with 0.75 mm reproducibility, which is an order of magnitude short of the required alignment accuracy if the sensors are 200 mm apart. Therefore, a better option are 328 329 distance sensors built from lasers with a shallow angle of incidence of 14°, which illuminate a 2 mm diameter spot 330 in the center underneath the coil at 25 mm distance from the coil surface and receive the reflected light with a 331 camera. A back-of-the-envelope calculation shows that an angle maladjustment of 0.25° will shift the center of the 332 reflected laser beam by 4 mm when laser and detector are 200 mm apart (Figs. 6, 7). This design will provide the 333 needed accuracy and precision for alignment at a fixed distance of 25 mm. Following parallel alignment of 334 sensitive slice and object surface, the gap between sensor and object can be shorted under control of the stepper 335 motor before starting the acquisition of a depth profile by retracting the sensor from the wall in defined steps 336 between measurements.

337 4.3 Operating software

338 To operate the equipment at locations with restricted spatial access (Fig. 5e) a wireless control strategy should be 339 followed. The two most important operations to be under remote control are the control of the stepper motor and 340 the data acquisition. A depth profile is typically acquired in two runs. A first profile is acquired at low spatial 341 resolution and signal-to-noise ratio to determine the exact location and depth range of interest. Subsequently, a 342 high-resolution profile is acquired with more scans per spot and smaller step size. Depending on the required 343 information and the time available, either full multi-echo decays are measured for further analysis in terms of 344 distributions of relaxation times, or only the first points of the decays are recorded to determine proton density 345 corresponding, for example, to volumetric moisture content. The measurement progress during depth profiling is 346 usually monitored in regular intervals to catch sporadic noise interference, uninformative data, and erroneous 347 parameter settings as budgeting time is important due to up to two hours long acquisition times for a depth profile 348 and limited access time in museums, historic buildings, and at excavation sites.

349 While operating the NMR-MOUSE appears to be a simple endeavor to most people with a basic 350 understanding of NMR relaxometry or MRI (Blümich et al., 2014; Johns et al., 2016), it is a true barrier to most 351 others interested in using it for materials testing. Therefore, the operating platform should avoid NMR jargon as 352 much as possible and relate the NMR acquisition parameters to object-specific information such as hard, soft, wet, 353 moist, dry, moisture content, component concentration, duration of measurement, etc., which have to be entered 354 by the operator. Prior to measurement, the proper functioning of the equipment needs to be checked, in particular, 355 the noise-level and the phase angle of the transverse magnetization. The proper functioning of the equipment and 356 potential faults should be flagged, and the receiver phase angle be adjusted automatically if needed. Moreover, it 357 should be possible to measure again particular depth ranges identified in previous scans. All raw data need to be 358 saved for later access and processing in expert mode. In addition to the data acquisition, the operating platform 359 needs to include data processing routines, that allow to derive depth profiles with different contrast types from the 360 acquired data, e. g. hydrogen concentration (spin density), relaxation (T_2) weighted spin density (w-parameter



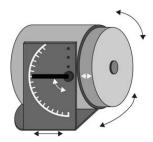


361 (Blümich et al., 2014)), peak integrals and peak ratios from distributions of relaxation times, as well as depth-

- 362 resolved distributions of relaxation times. The latter requires access to an inverse Laplace transform algorithm.
- 363 Finally, it should be possible to display the data from several measurements at the same scales for comparison and
- 364 interpretation of results.

365 4.4 Mounting device and scaffold

Given the dimensions of the magnets (Fig. 6a,b), the weight of the sensor is estimated to approach 40 kg. For depth profiling, the device first needs to be positioned with high accuracy at 0.5 to 1 mm away from the surface of the object, so that depth profiles can be scanned by retracting the sensor between scans in small, preset steps of typically 0.05 to 0.25 mm. This way of scanning assures that the object is not damaged by setting a wrong depth range. The mounting device has to enable manual fine adjustment of the sensor orientation following the readings of the alignment sensors and allow stable positioning of the sensor at various angles with high precision for long times from tens of minutes to a few hours.



374

375 Figure 8. Conceptual drawing of a sensor mounting device.

376

377 A simple mounting device fulfilling these criteria would consist of a U-shaped aluminum frame (Fig. 8). It 378 would have a flat, felt- or plastic-covered bottom without legs. Position and orientation would be adjusted 379 manually (arrows). To access all polar angles, the polar rotation axis would be adjustable to different values in the 380 device, and one would be able to turn the entire device upside down. To balance the sensor during depth profiling, 381 the horizontal position of the polar rotation axis would be at the average center of gravity for a 20 mm shift range. 382 The bottom plate would be extended at the back to provide a location for clamping the device to a scaffold or table. 383 For most studies outside the lab a modular scaffold had been employed (Fig. 4a), which can be assembled 384 from aluminum tubing with plastic joints in different ways to position the sliding table carrying the NMR-MOUSE 385 at different heights up to about two meters. Each of the three scaffold legs consists of two telescoped tubes so that 386 the legs are extendable via a long, threaded bolts which move the inner tubes in an out by rotating the bolt heads 387 from the top with a cordless electric drill. While this scaffold serves its purpose and is easy to transport and set up, 388 the scaffold is sensitive to vibrations and torsion. Moreover, it would be helpful to be able to adjust its height from 389 the bottom and not the top and with the sensor in place, in particular, when high positions need to be accessed.

390 5. Summary

Single-sided NMR relaxometry is a technique for nondestructive materials testing. Instruments like the NMR MOUSE have been developed for use in the laboratory. Applications are found in quality control and aging of





393 polymers and related materials, including PE pipes, PVC flooring, car tires, asphalt pavements, human skin, and 394 food products. The dead time of the current sensors limits the detection of rapidly decaying transverse 395 magnetization, e. g. from bound water in building materials like cement, from glass- and carbon-fiber-reinforced 396 polymer composites in windmill wings, and varnish on paintings and musical instruments. In addition to that, in 397 many cases, measurements need to be conducted at different depths or complete depth profiles need to be acquired. 398 This is the case, e.g., for moisture in walls, where NMR is one if not the only method that directly measures 399 quantitative water content without averaging over depth ranges where the moisture content significantly varies. 400 Emerging applications in cultural heritage studies demand equipment that can easily be transported, set up, and 401 operated. This equipment needs to small and robust. The childhood and adolescence of the NMR-MOUSE 402 equipment have been reviewed and parental advice given for preparation of outdoor measurements and survival 403 outside the protected childhood home.

404

405 References

| 406 | Anders, J., Handwerker, J., Ortmanns, M., Boero, G.: A low-power high-sensitivity single-chip receiver for, NMR |
|-----|--|
| 407 | microscopy, J. Magn. Reson. 266, 41-50, 2017. |
| 408 | Anders, J.; Work in progress, 2020. |
| 409 | Anferova, S., Anferov, V., Adams, M., et al.: Construction of a NMR-MOUSE with Short Dead Time, Concepts |
| 410 | Magn. Reson. B 15, 15–25, 2002. |
| 411 | Angelova, L. V., Ormsby, B., Richardson, E.: Diffusion of water from a range of conservation treatment gels into |
| 412 | paint films studied by unilateral NMR: Part I: Acrylic emulsion paint, Microchem. J. 124, 311-320, 2016. |
| 413 | Armstrong-Smith, I.: A Briefcase Full of NMR, The Analytical Scientist, 26, 24-31, 2015. |
| 414 | Baias, M., Blümich, B.: Nondestructive testing of objects from cultural heritage with NMR, in: G.A. Webb, |
| 415 | Modern Magnetic Resonance, https://doi.org/10.1007/978-3-319-28275-6_29-1, 2017. |
| 416 | Balibanu, F., Hailu, K., Eymael, R., Demco, D. E., Blümich, B.: Nuclear Magnetic Resonance in inhomogeneous |
| 417 | fields, J. Magn. Reson. 145, 248–258, 2000. |
| 418 | Blümich, B., Anferov, V., Anferova, et al.: Simple NMR-MOUSE with a Bar Magnet, Concepts Magn. Reson.: |
| 419 | Magn. Reson. Eng, 15, 155–261, 2002. |
| 420 | Blümich, B., Baias, M., Rehorn, C., et al., Comparison of historical violins by non-destructive MRI depth profiling, |
| 421 | Microchemical Journal 158, 105219, 2020. |
| 422 | Blümich, B., Bruder, M., Guerlin, T., Prado, P.: Device for inspecting flat goods made of polymeric materials with |
| 423 | embedded textile strength supports, patent WO200079253A1, 20 June 1999. |
| 424 | Blümich, B., Casanova, F., Perlo, J., et al.: Noninvasive testing of art and cultural heritage by mobile NMR, Acc. |
| 425 | Chem. Res. 43, 761–770, 2010. |
| 426 | Blümich, B., Haber-Pohlmeier, S., Zia, W.: Compact NMR, de Gruyter, Berlin, 2014. |
| 427 | Blümich, B., Kölker, C., Casanova, F., Perlo, J., Felder, J.: Ein mobiler und offener Kernspintomograph: |
| 428 | Kernspintomographie für Medizin und Materialforschung, Physik in unserer Zeit 36, 236–242, 2005. |
| 429 | Blümich, B., Perlo, J., Casanova, F.: Mobile single-sided NMR, Prog. Nucl. Magn. Reson. Spectr. 52, 197-269, |
| 430 | 2008. |





| 431 | Blümich, B., Singh, K.: Desktop NMR and its applications from materials science to organic chemistry, Angew. |
|-----|--|
| 432 | Chem. Int. Ed. Eng. 57, 6996–7010, 2018. |
| 433 | Blümich, B., Teymouri, Y., Clark, R.: NMR on the Road: Non-destructive Characterization of the Crumb-Rubber |
| 434 | Fraction in Asphalt, Appl. Magn. Reson. 50 497-509, 2019. |
| 435 | Blümich, B.: Concepts and Applications of the NMR-MOUSE, in: Bastidas, D. M., Cano, E.: Advanced |
| 436 | Characterization Techniques, Diagnostic Tools and Evaluation Methods in Heritage Science, Springer, |
| 437 | Cham, 61–79, 2019. |
| 438 | Blümich, B.: Essential NMR for Scientists and Engineers, 2 nd ed., Springer, Cham, 2019. |
| 439 | Blümich, B.: Low-field and benchtop NMR, J. Magn. Reson. 306, 27-35, 2019. |
| 440 | Blümich, B.: Miniature and Tabletop Nuclear Magnetic Resonance Spectrometers, Enc. Anal. Chem. a9458, 1- |
| 441 | 31, 2016. |
| 442 | Blümich, B.: NMR Imaging of Materials, Clarendon Press, Oxford, 2000. |
| 443 | Blümich, B.: The Incredible Shrinking Scanner, Scientific American 299, 92-98 2008. |
| 444 | Bürkle, H., Schmid, K., Klotz, T., Krapf, R., Anders, J.: A high voltage CMOS transceiver for low-field NMR |
| 445 | with a maximum output current of 1.4 App, 2020 IEEE International Symposium on Circuits and Systems |
| 446 | (ISCAS), 10–21 Oct., 10.1109/ISCAS45731.2020.9181025, 2020. |
| 447 | Busse, F., Rehorn, C., Küppers, M., et al.: NMR relaxometry of oil paint binders, Magn. Reson. Chem. 58, 830- |
| 448 | 839, 2020. |
| 449 | Callaghan, P. T., Eccles, C. D., Haskell, T. G., Langhorne, P. J., Seymour, J. D.: Earth's Field NMR in Antarctica: |
| 450 | A Pulsed Gradient Spin Echo NMR Study of Restricted Diffusion in Sea Ice, J. Magn. Reson. 133, 148–154, |
| 451 | 1998. |
| 452 | Capitani, D., Di Tullio, V., Proietti, N.: Nuclear magnetic resonance to characterize and monitor cultural heritage, |
| 453 | Prog. Nucl. Magn. Reson. Spectrosc. 64, 29-69, 2012. |
| 454 | Capitani., D., Sobolev, A., Di Tullio, V. D., Mannina, L., Proietti, N.: Portable NMR in food analysis, Chem. Biol. |
| 455 | Technol. Agric. 4, 1–14, 2017. |
| 456 | Casanova, F., Blümich, B.: Two-dimensional imaging with a single-sided NMR probe, J. Magn. Reson. 163, 38- |
| 457 | 45, 2003. |
| 458 | Casanova, F., Perlo, J., Blümich, B., eds.: Single-Sided NMR, Springer, Berlin, 2011. |
| 459 | Chu, A., Schlecker, B., Handwerker, J., et al.: VCO-based ESR-on-a-chip as a tool for low-cost, high-sensitivity |
| 460 | food quality control, IEEE Biomedical Circuits and Systems Conference (BioCAS), Turin, 1-4, 2017, doi: |
| 461 | 10.1109/BIOCAS.2017.8325172, 2017. |
| 462 | Coates G. R., Xiao, L., Prammer, L. G.: NMR Logging Principles and Applications, Halliburton, Houston, 1999. |
| 463 | Dalitz, F., Cudaj, M., Maiwald, M., Guthausen, G.: Process and reaction monitoring by low-field NMR |
| 464 | spectroscopy, Prog. Nucl. Magn. Reson. Spectrosc. 60, 52–70. |
| 465 | Danieli, E., Perlo, J., Blümich, B., Casanova, F.: Small magnets for portable NMR spectrometers, Angew. Chem. |
| 466 | Int. Ed. 49, 4133–4135, 2010. |
| 467 | Eidmann, G., Savelsberg R., Blümler, P., Blümich, B.: The NMR MOUSE, a mobile universal surface explorer, |
| 468 | J. Magn. Reson. A122,104–109, 1996. |
| 469 | Fife, G. R., Stabik, B., Kelley, A. E., et al.: Characterization of aging and solvent treatments of painted surfaces |
| 470 | using single-sided NMR, Magn. Reson. Chem. 53, 58–63, 2015. |

14





| 471 | Fukushima, E.: Introduction, in: Johns, M. L., Fridjohnsson, E. O., Vogt, J. J., Haber, A., eds.: Mobile NMR and |
|---|--|
| 472 | MRI: Developments and Applications, Royal. Soc. Chem., Cambridge, 1-10, 2016. |
| 473 | Grisi, M., Gualco, G., Boero, G.: A Broadband Single-chip Transceiver for Multi-nuclear NMR Probes, Rev. Sci. |
| 474 | Instrum. 86, 044703, 2015. |
| 475 | Gutowsky, H. S., Meyer, L.H., McClure, R. E.: Apparatus of Nuclear magnetic Resonance, Rev. Sci. Instrum. 24, |
| 476 | 644–652, 1953. |
| 477 | Ha, D., Paulsen, J., Sun, N., Song, YQ., Ham, D.: Scalable NMR Spectroscopy with Semiconductor Chips, Proc. |
| 478 | Nat. Acad. Sci. 111, 11955–11960, 2014. |
| 479 | Ha, D., Sun, N., Ham, D.: Next-Generation Multidimensional NMR Spectrometer Based on Semiconductor |
| 480 | Technology, eMagRes 4, 117-126, 2015. |
| 481 | Hailu, K., Fechete, R., Demco, D. E., Blümich, B.: Segmental anisotropy in strained elastomers detected with a |
| 482 | portable NMR scanner, Solid State Nucl. Magn. Reson. 22, 327-343, 2002. |
| 483 | Haken, R., Blümich, B.: Anisotropy in Tendon Investigated in Vivo by a Portable NMR Scanner, the NMR- |
| 484 | MOUSE, J. Magn. Reson. 144, 195–199, 2000. |
| 485 | Hürlimann, M. D., Griffin, D. D.: Spin Dynamics of Car-Purcell-Meiboom-Gill-like sequences in grossly |
| 486 | inhomogeneous B_0 and B_1 fields and applications to NMR well logging, J. Magn. Reson. 143, 120–135, |
| 487 | 2000. |
| 488 | Jackson J. A., Burnett, L. J., Harmon, J. F.: Remote (inside-out) NMR. III. Detection of nuclear magnetic |
| 489 | resonance in a remotely produced region of homogeneous magnetic field, J. Magn. Reson. 41, 411-421, |
| 490 | 1980. |
| 491 | Johns, M. L., Fridjohnsson, E. O., Vogt, J. J., Haber, A., eds.: Mobile NMR and MRI: Developments and |
| 102 | Applications, Royal. Soc. Chem., Cambridge, 2016. |
| 492 | |
| 493 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous |
| 493 494 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). |
| 493 494 495 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019).Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous |
| 493 494 495 496 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE |
| 493 494 495 496 497 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. |
| 493 494 495 496 497 498 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. |
| 493 494 495 496 497 498 499 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. |
| 493 494 495 496 497 498 499 500 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. |
| 493 494 495 496 497 498 499 500 501 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging |
| 493 494 495 496 497 498 499 500 501 501 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. |
| 493 494 495 496 497 498 499 500 501 502 503 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field |
| 493 494 495 496 497 498 499 500 501 502 503 503 504 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field Gradient (Mini-MOUSE), Appl. Magn. Reson. 46, 181–202, 2015. |
| 493 494 495 496 497 498 499 500 501 502 503 504 505 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field Gradient (Mini-MOUSE), Appl. Magn. Reson. 46, 181–202, 2015. Oligschläger, D., Kupferschläger, K., Poschadel, T., Watzlaw, J., Blümich, B.: Miniature mobile NMR sensors |
| 493 494 495 496 497 498 499 500 501 502 503 503 504 505 506 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field Gradient (Mini-MOUSE), Appl. Magn. Reson. 46, 181–202, 2015. Oligschläger, D., Kupferschläger, K., Poschadel, T., Watzlaw, J., Blümich, B.: Miniature mobile NMR sensors for material testing and moisture-monitoring, Diffusion Fundamentals 22, 1–25, 2014. |
| 493 494 495 496 497 498 499 500 501 502 503 504 505 506 507 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field Gradient (Mini-MOUSE), Appl. Magn. Reson. 46, 181–202, 2015. Oligschläger, D., Kupferschläger, K., Poschadel, T., Watzlaw, J., Blümich, B.: Miniature mobile NMR sensors for material testing and moisture-monitoring, Diffusion Fundamentals 22, 1–25, 2014. Olmi, R., Bini, M., Ignesti, A., et al.: Diagnostics and monitoring of frescoes using evanescent-field |
| 493 494 495 496 497 498 499 500 501 502 503 503 504 505 506 | Kern, S., Wander, L., Meyer, K., et al.: Flexible automation with compact NMR spectroscopy for continuous production of pharmaceuticals, Anal. Bioanal. Chem. 411, 3037–3046 (2019). Keschenau, P. R., Klingel, H., Reuter, S., et al.: Evaluation of the NMR-MOUSE as a new method for continuous functional monitoring of the small intestine during different perfusion states in a porcine model, PLOS ONE 0206697, 1–17, 2018. Kleinberg, R. L., Jackson, J.A.: An Introduction to the History of NMR Well Logging, Concepts Magn. Reson. 13, 340–342, 2001. Nordon, A., McGill, C. A., Littlejohn, D.: Process NMR spectrometry, Analyst 126, 260–272, 2001. Oligschläger D., Lehmkuhl, S., Watzlaw, J., et al.: Miniaturized multi-coil arrays for functional planar imaging with a single-sided NMR sensor, J. Magn. Reson. 254–18, 2015. Oligschläger, D., Glöggler, S., Watzlaw, J., et al.: A Miniaturized NMR-MOUSE with a High Magnetic Field Gradient (Mini-MOUSE), Appl. Magn. Reson. 46, 181–202, 2015. Oligschläger, D., Kupferschläger, K., Poschadel, T., Watzlaw, J., Blümich, B.: Miniature mobile NMR sensors for material testing and moisture-monitoring, Diffusion Fundamentals 22, 1–25, 2014. |

510 1110–1112, 2006.





| 511 | Perlo, J., Casanova, F., Blümich, B.: Profiles with microscopic resolution by single-sided NMR, J. Magn. Reson. |
|-----|---|
| 512 | 176, 64–70, 2005. |
| 513 | Perlo, J., Demas, V., Casanova, F., et al.: High-resolution NMR spectroscopy with a portable single-sided sensor, |
| 514 | Science 308, 1229, 2005. |
| 515 | Prati, S., Sciutto, G., Volpi, F., et. al.: Cleaning oil paintings: NMR relaxometry and SPME to evaluate the effects |
| 516 | of green solvents and innovative green gels, N. J. Chem. 43, 8229-8238, 2019. |
| 517 | Presciutti, F., Perlo, J., Casanova, F., et al.: Noninvasive nuclear magnetic resonance profiling of painting layers, |
| 518 | Appl. Phys. Lett. 93, 033505, 2008. |
| 519 | Proietti, N., Capitani, D., Rossi, E., Cozzolino, S., Segre, A. L.: Unilateral NMR study of a XVI century wall |
| 520 | painted, J. Magn. Reson. 186, 311-318, 2007. |
| 521 | Rehorn, C., Blümich, B.: Cultural Heritage Studies with Mobile NMR, Angew. Chem. Int. Ed. Eng. 57, 7304- |
| 522 | 7312, 2018. |
| 523 | Rehorn, C., Kehlet, C., Del Federico, E., et al.: Automatizing the comparison of NMR depth profiles, Strain 54, |
| 524 | e12254, 2018. |
| 525 | Rühli, F., Böni, T., Perlo, J., et al.: Non-invasive spatial tissue discrimination in ancient mummies and bones in |
| 526 | situ by portable nuclear magnetic resonance, J. Cultural Heritage 8, 257-263, 2007. |
| 527 | Saalwächter, K., Microstructure and dynamics of elastomers as studied by advanced low-resolution NMR |
| 528 | methods, Rubber Chem. Tech. 85, 350-386, 2012. |
| 529 | Segre, A. L., Blümich, B.: Progetto 'MOUSE': Risonanza magnetica per i beni culturali, Ricerca & Futuro 25, 34- |
| 530 | 36, 2002. |
| 531 | Van Landeghem, M., Danieli, E., Perlo, J., Blümich, B., Casanova, F.: Low-gradient single-sided NMR sensor for |
| 532 | one-shot profiling of human skin, J. Magn. Reson. 215, 74-84, 2012. |
| 533 | van Putte, K., van den Enden, J.: Fully automated determination of solid fat content by pulsed NMR, J. Am. Oil |
| 534 | Chem. Soc. 51 316–320, 1974. |
| 535 | Varian, R. H.: Apparatus and Method for Identifying Substances, US patent 2,651,490, filed 3 January 1952. |
| 536 | Watzlaw, J., Glöggler, S., Blümich, B., Mokwa, W., Schnakenberg, U.: Stacked planar micro coils for single-sided |
| 537 | NMR applications, J. Magn. Reson. 230, 176-185, 2013. |
| 538 | Woessner, D. E.: The Early Days of NMR in the Southwest, Concepts Magn. Reson. 13, 77-102, 2001. |
| 539 | Zalesskiy, S.S., Danieli, E., Blümich, B., Ananikov, V. P.: Miniaturization of NMR systems: desktop |
| 540 | spectrometers, microcoil spectroscopy, and "NMR on a chip" for chemistry, biochemistry, and industry, |
| | |

541 Chem. Rev. 114, 5641–5694 (2014).